

4D magnetic resonance velocimetry and numerical simulations for studying helical flows in cerebral blood vessels

**Alexander Khe, V. Vanina, A. Cherevko,
D. Parshin, A. Tulupov, A. Chupakhin**

Lavrentyev Institute of Hydrodynamics, Novosibirsk, Russia

Novosibirsk State University, Novosibirsk, Russia

International Tomography Center, Novosibirsk, Russia

The Week of Applied Mathematics and Mathematical Modelling
October 7–11, 2019, FEFU, Vladivostok, Russia

Supported by the Russian Science Foundation (Grant No. 17-11-01156)

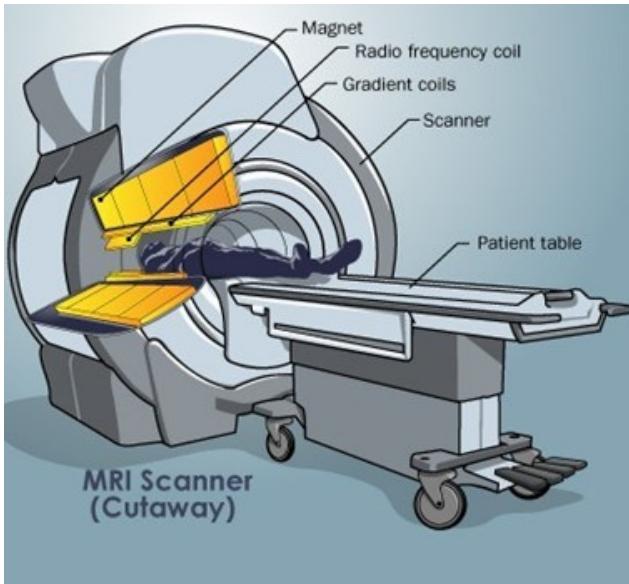
Study of blood flow

- Non-invasive methods:
 - Doppler ultrasonography
 - Computed tomography (CT)
 - Magnetic resonance imaging (MRI)
- MRI — heart
 - L. A. Bokeria, et al., 2013
- MRI — aorta
 - A. Frydrychowicz, et al., 2009
 - M. Markl, et al., 2010
- Ultrasonography — CCA bifurcation
 - V. P. Kulikov, R. I. Kirsanov, 2013
 - A. D. Yukhnev, Ya. A. Gataulin, et al., 2015

Aim

- Investigation of the velocity field of physiological flows with MRI:
 - Development of the research protocol
 - Development of the post-processing software
- Study of flood flow helicity in cerebral vessels
- Study of blood and cerebrospinal fluid flows

Experimental setup



3-tesla MR scanner Philips Ingenia 3T



Common carotid artery bifurcation
(Shelley Medical Imaging Technologies)



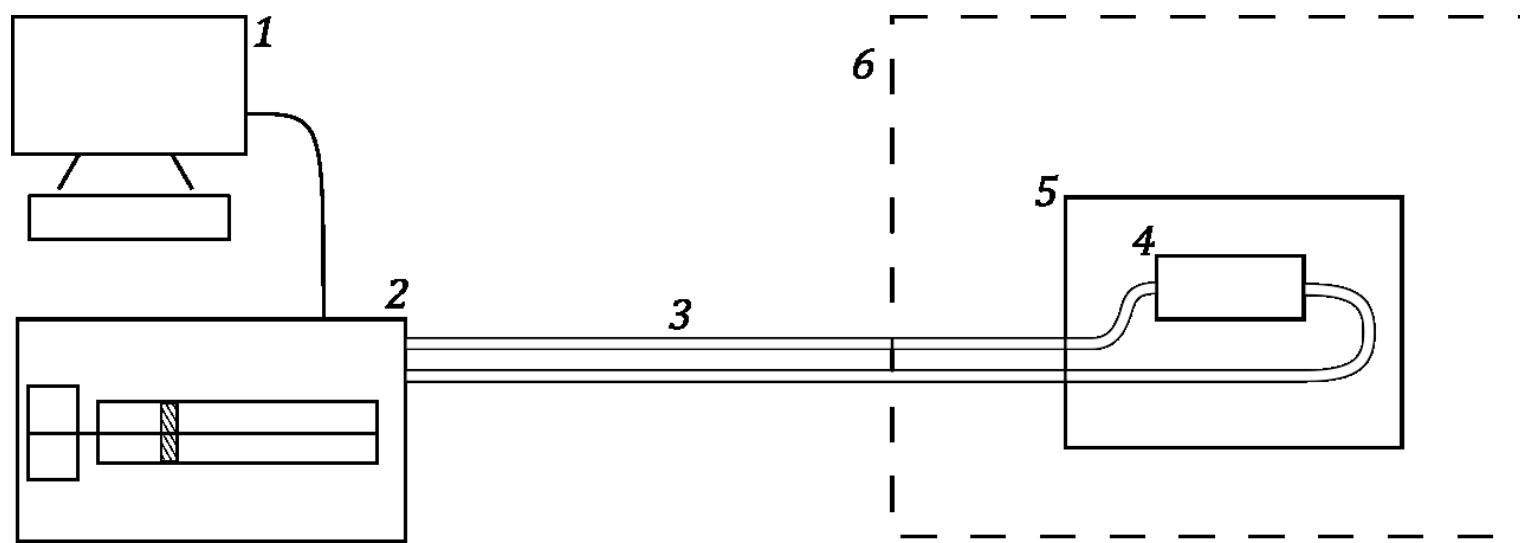
Programmable pump CompuFlow 1000MR
(Shelley Medical Imaging Technologies)



Giant aneurysm on
internal carotid artery
(Shelley Medical
Imaging Technologies)

Blood mimicking liquid: glycerol solution
(density 1000 kg/m³, viscosity 0,004 Pa·s)

Experimental setup



1 — computer

2 — programmable pump

3 — connecting tubes

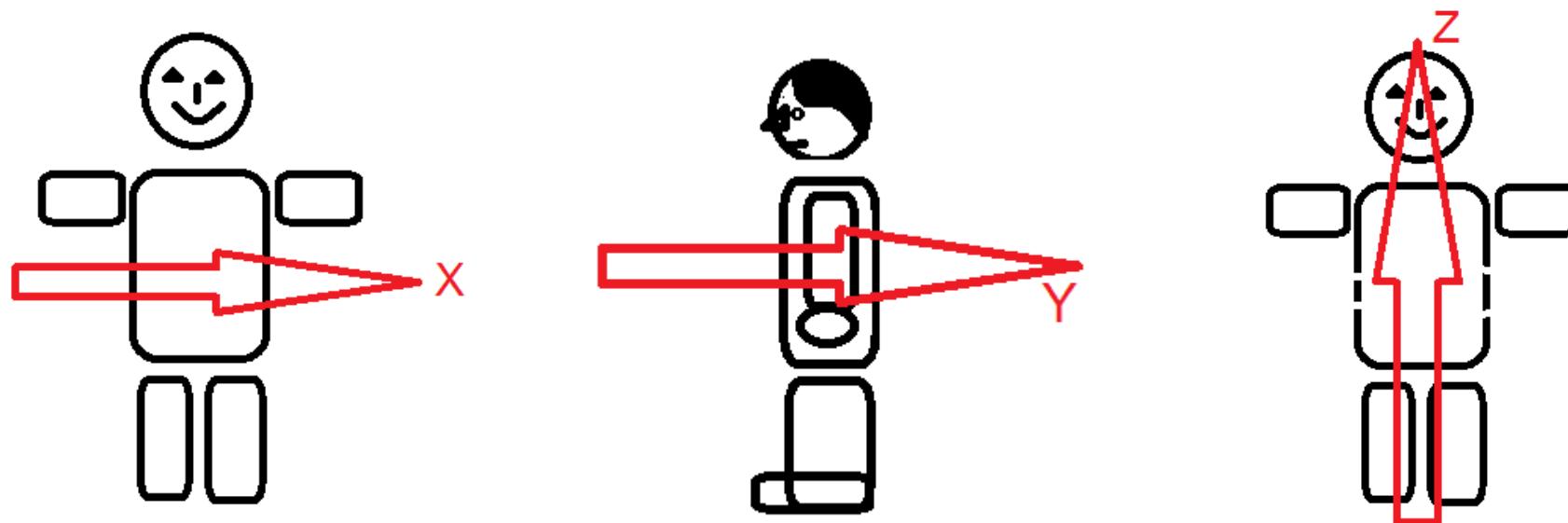
4 — vessel model

5 — MR scanner

6 — shield (Faraday cage)

Reconstruction of the velocity field (4D Qflow)

- Each measurement in 4D Qflow results in 4 series of DICOM images
 - PCA/P-RL — x
 - PCA/P-AP — y
 - PCA/P-FH — z



- Metadata: image position, image orientation, spacing between slices, pixel spacing, time step number, trigger time
- ImageOrientation — rotation matrix

DICOM images



Fluid (proton) density image



Velocity component
(three Cartesian components)

Comparison of the measurements*

Philips Achieva 1.5 T



Medical MR scanner

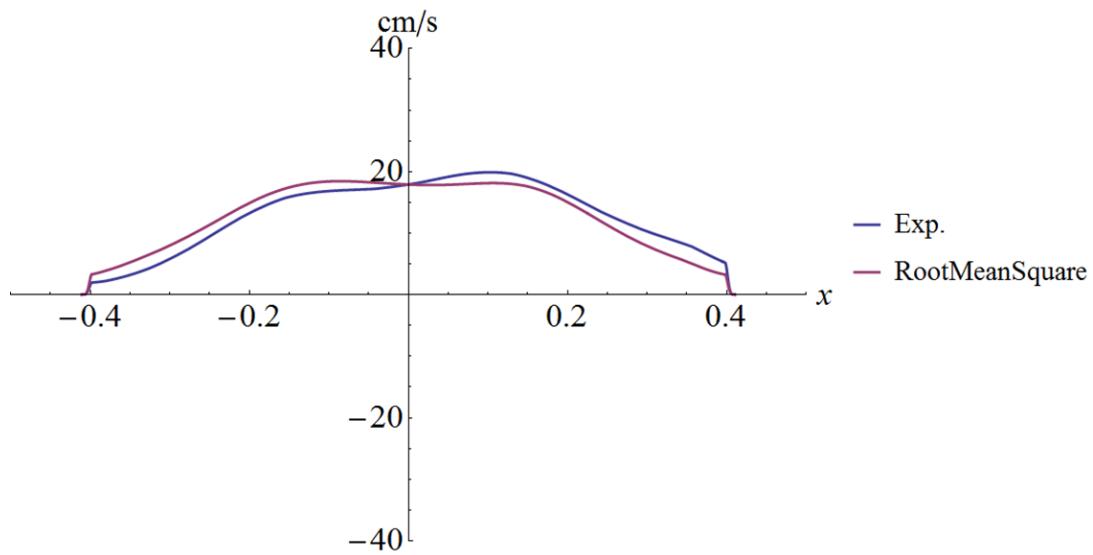
Bruker BioSpec 117/16 USR 11.7 T



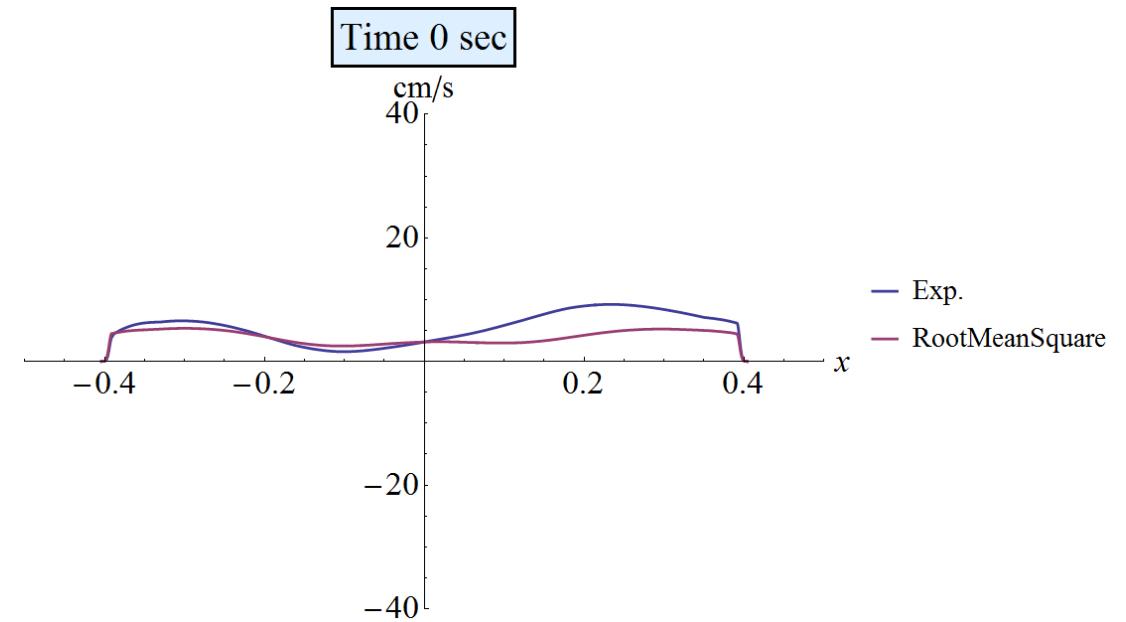
Research MR scanner

Velocity profile (Philips 1.5 T)

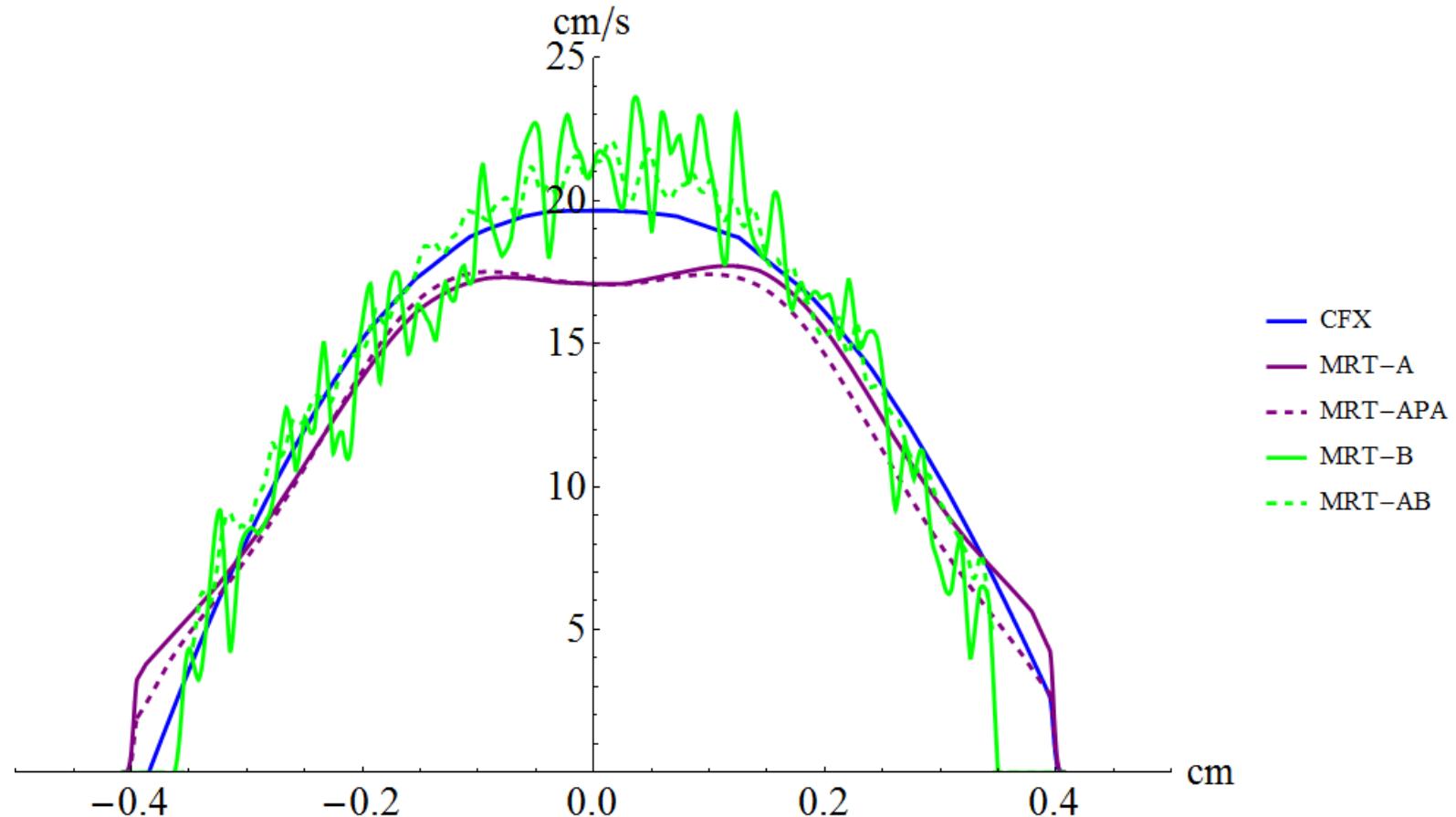
Stationary flow 5 ml/s



Non-stationary flow $0.1 + 10 \sin(\pi t)$



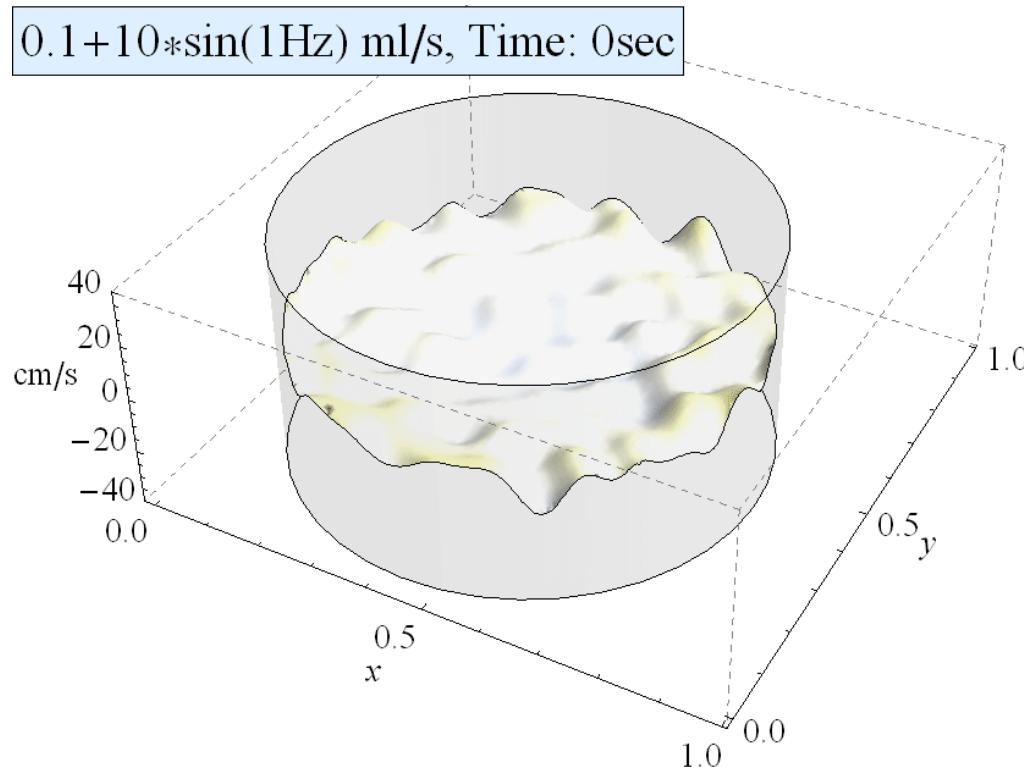
Stationary flow, 5 ml/s



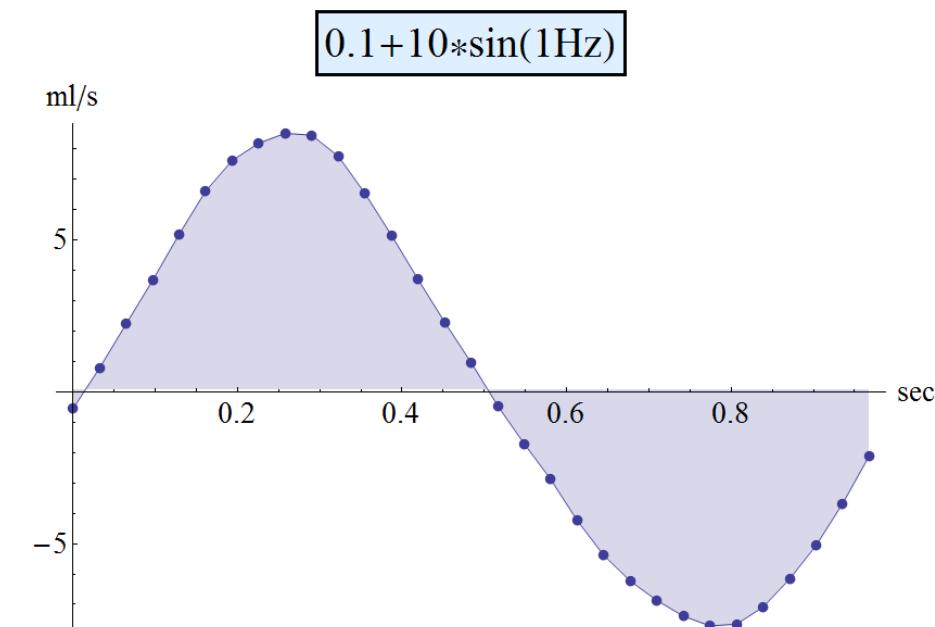
Comparison of the results obtained by numerical simulation and MRI: **violet** – Philips, **green** – Bruker.

Non-stationary flow (Philips 1.5 T)

Velocity profile

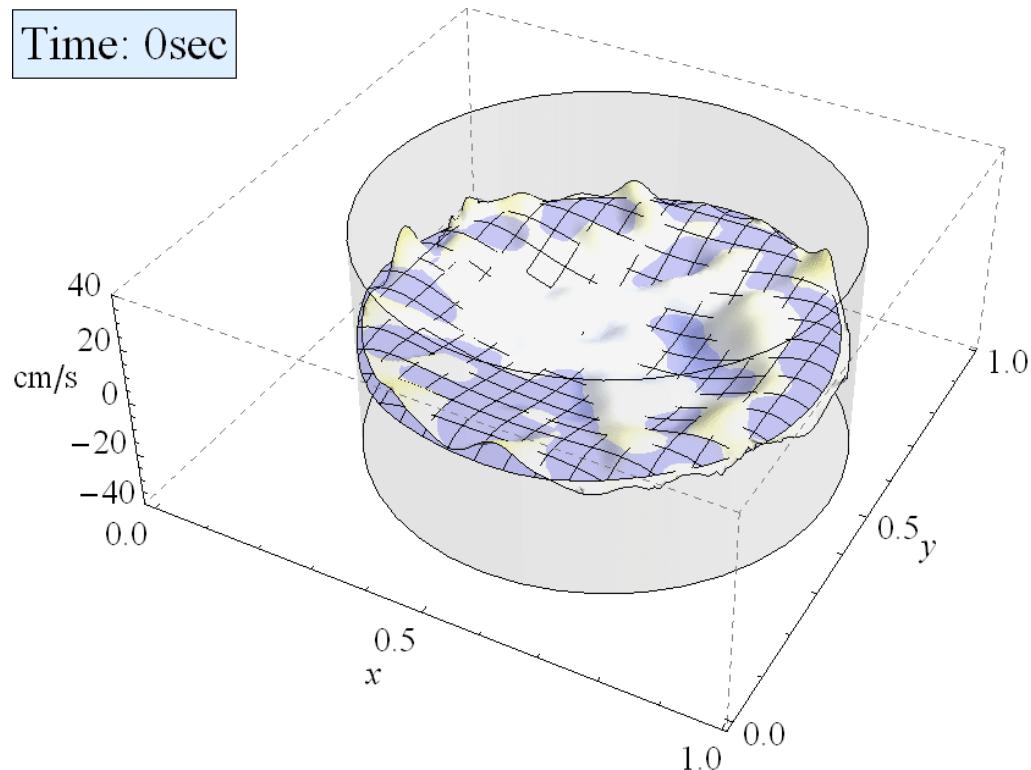


Flow rate

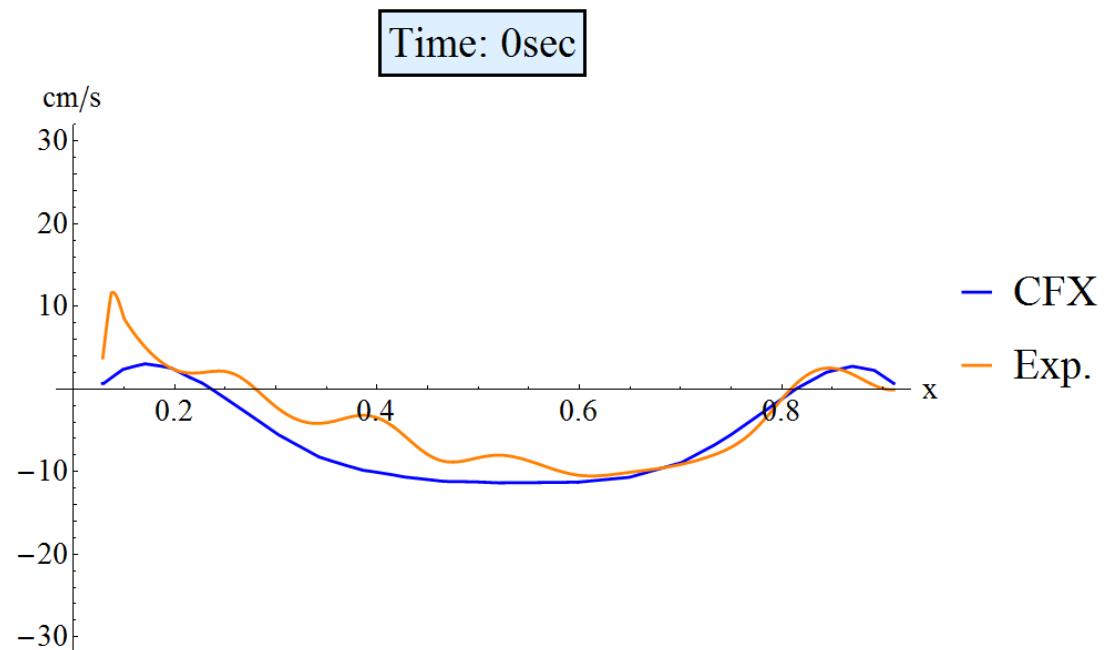


Non-stationary flow $0.1 + 10 \sin(\pi t)$ ml/s

Velocity profile

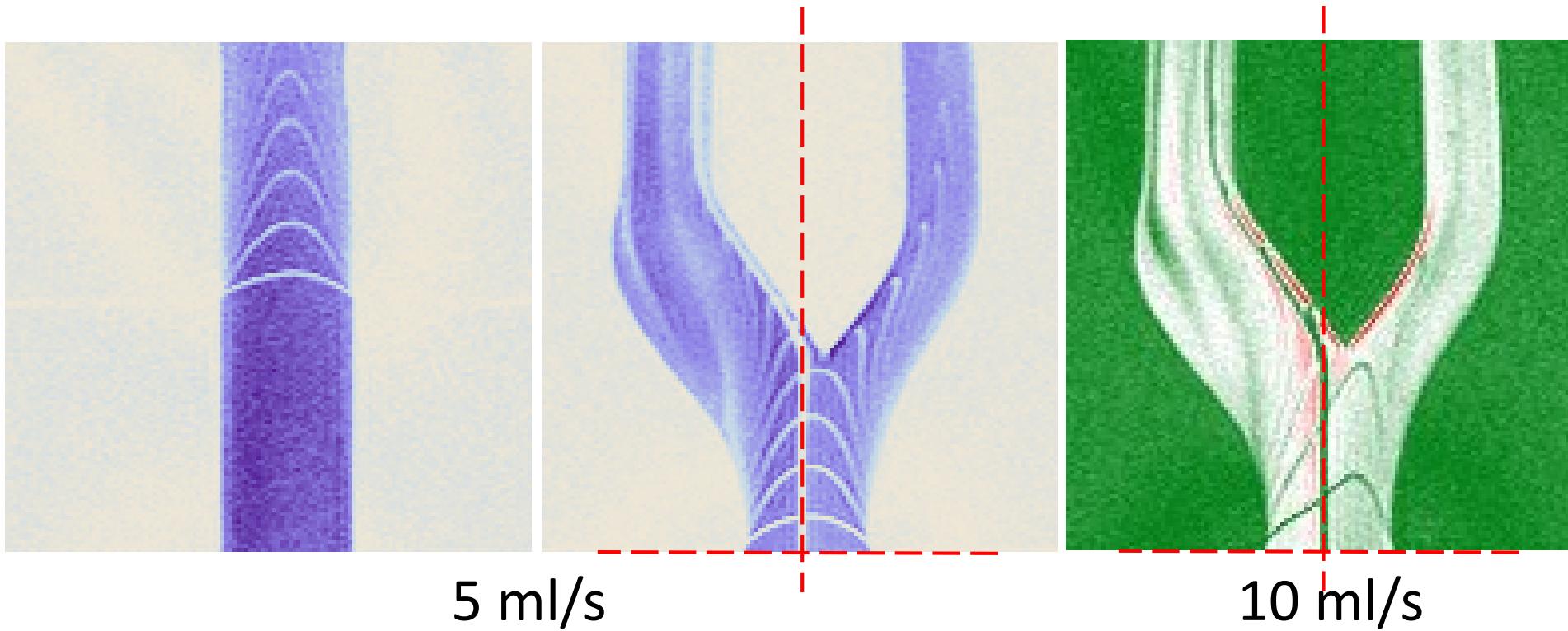


Averaged velocity profile



Comparison with numerical simulation

Fluid surfaces in stationary flow (Bruker 11.7 T)

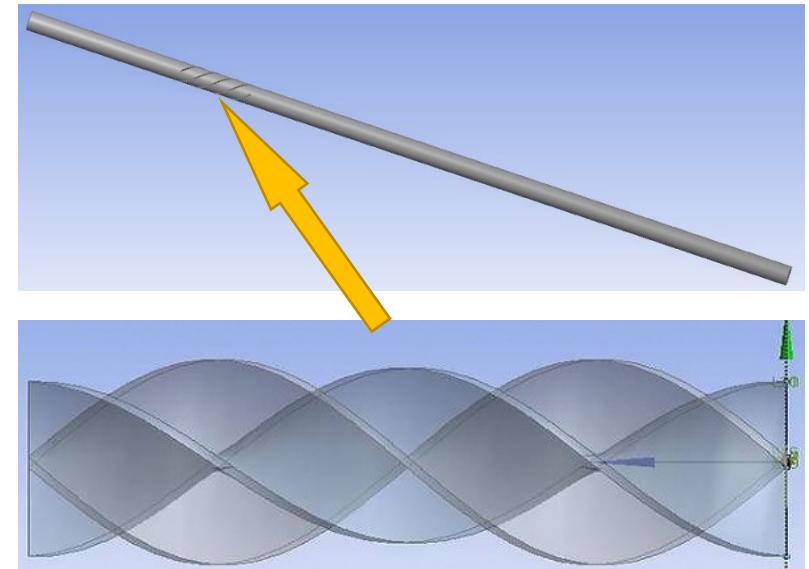


Experiments 4D Qflow

Session 1				
	1	Swirl generator v.1	$96 \times 96 \times 7$ (280)	18 ± 3 ml/s, 0.5 Hz
Session 2				
	a	Swirl generator v.1	$160 \times 160 \times 11$ (440)	18 ± 3 ml/s, 0.5 Hz
	b	Swirl generator v.1	$160 \times 160 \times 11$ (440)	18 ± 3 ml/s, 0.5 Hz
	c	Swirl generator v.1	$240 \times 240 \times 20$ (800)	18 ± 3 ml/s, 0.5 Hz
Session 3				
	1	Swirl generator v.1	$96 \times 96 \times 7$ (280)	18 ± 3 ml/s, 0.5 Hz
	2	Swirl generator v.1	$160 \times 160 \times 11$ (440)	18 ± 3 ml/s, 0.5 Hz
Session 4				
	2a	Swirl generator v.1	$96 \times 96 \times 7$ (280)	18 ± 3 ml/s, 0.5 Hz
	2b	Swirl generator v.1	$160 \times 160 \times 11$ (440)	18 ± 3 ml/s, 0.5 Hz
	2c	Swirl generator v.1	$240 \times 240 \times 20$ (800)	18 ± 3 ml/s, 0.5 Hz
	3a	Swirl generator v.2	$96 \times 96 \times 7$ (280)	18 ± 3 ml/s, 0.5 Hz
	3b	Swirl generator v.2	$160 \times 160 \times 11$ (440)	18 ± 3 ml/s, 0.5 Hz
Session 5				
	1	Aneurysm model	$176 \times 176 \times 25$ (1000)	12 ± 3 ml/s, 0.5 Hz
	2	Aneurysm model	$176 \times 176 \times 25$ (1000)	15 ± 3 ml/s, 0.5 Hz
Session 6				
	1	Aneurysm model	$176 \times 176 \times 25$ (1200)	15 ± 3 ml/s, 0.5 Hz
	2	CCA bifurcation	$96 \times 96 \times 7$ (280)	15 ± 3 ml/s, 0.5 Hz
	3	CCA bifurcation	$160 \times 160 \times 11$ (440)	15 ± 3 ml/s, 0.5 Hz

Flow in elastic tube

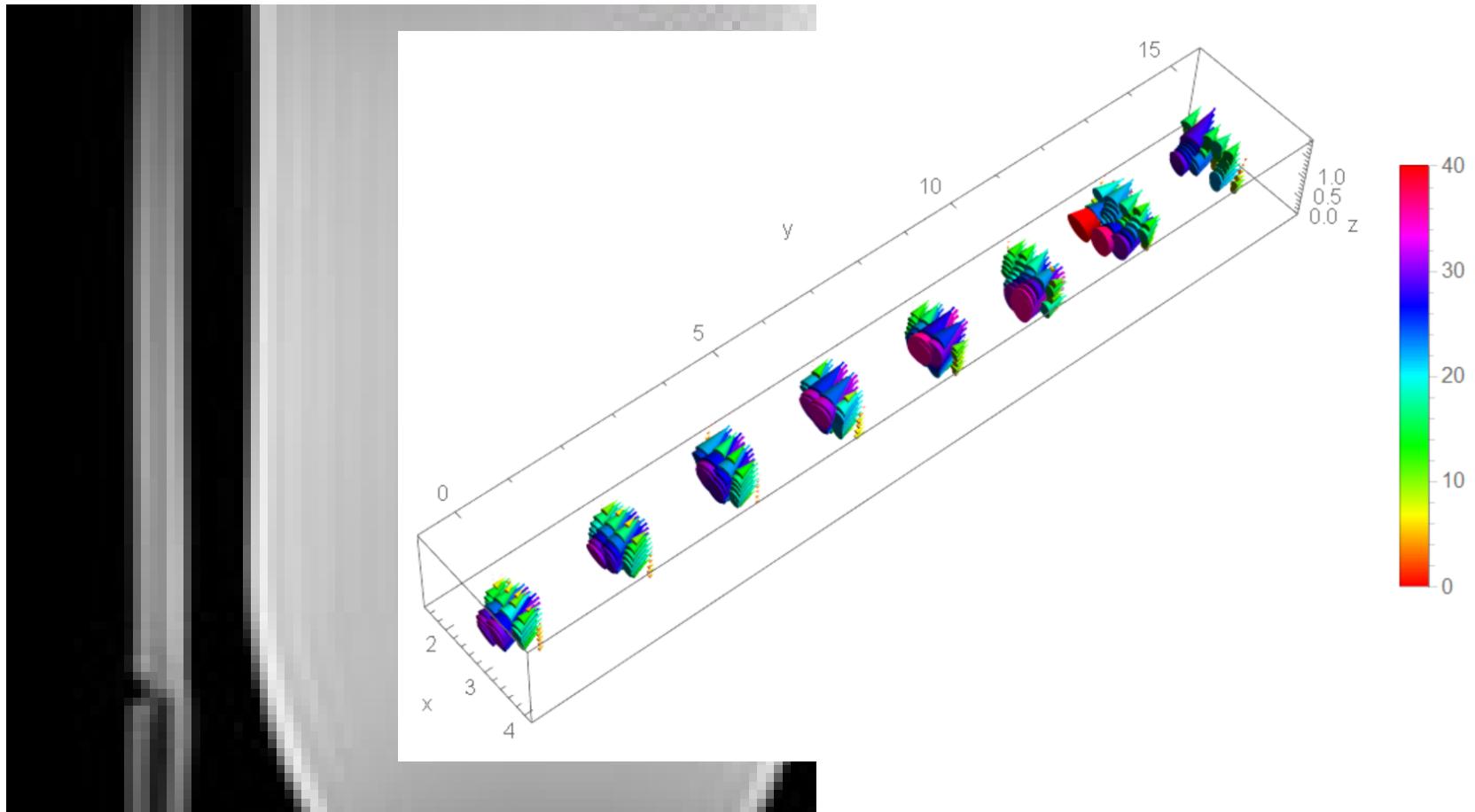
- Silicone tube with a swirl generator
- Flow rate: $18 + 3 \sin(\pi t)$ ml/s, $f = 0.5$ Hz.



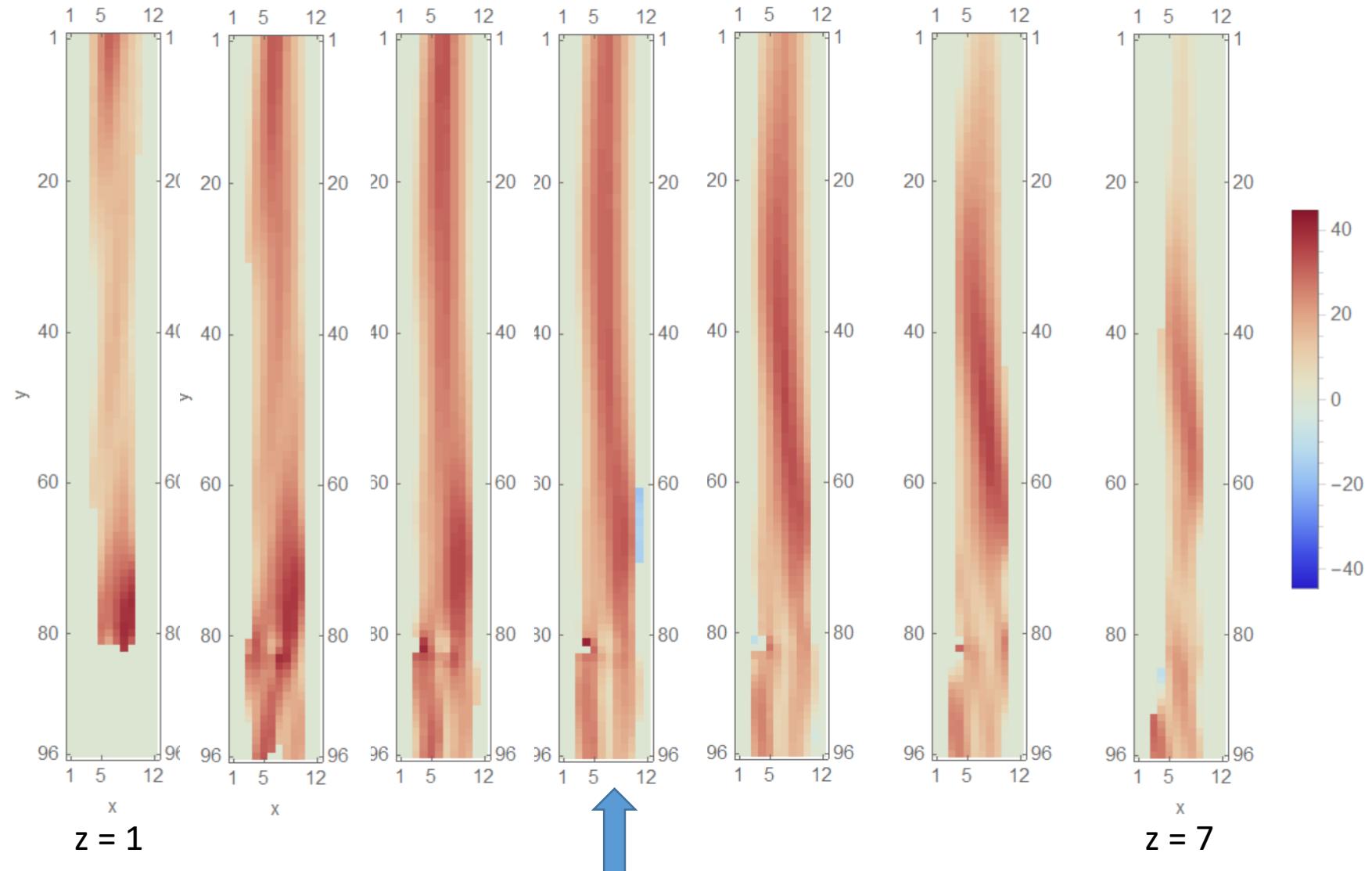
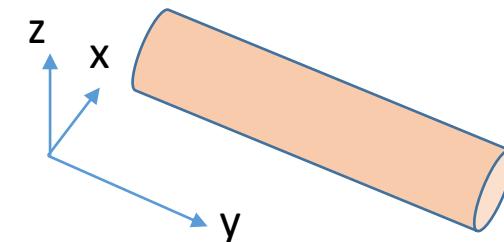
Silicone tube with swirl generator

3D matrix	Time steps	Voxel, mm ³	Domain, mm ³	Files
96×96×7	20	1.56×1.56×1.5	150×150×10.5	4 × 280
160×160×11	20	0.94×0.94×1.25	150×150×13.75	4 × 440
240×240×20	20	1.25×1.25×1.25	300×300×25	4 × 800

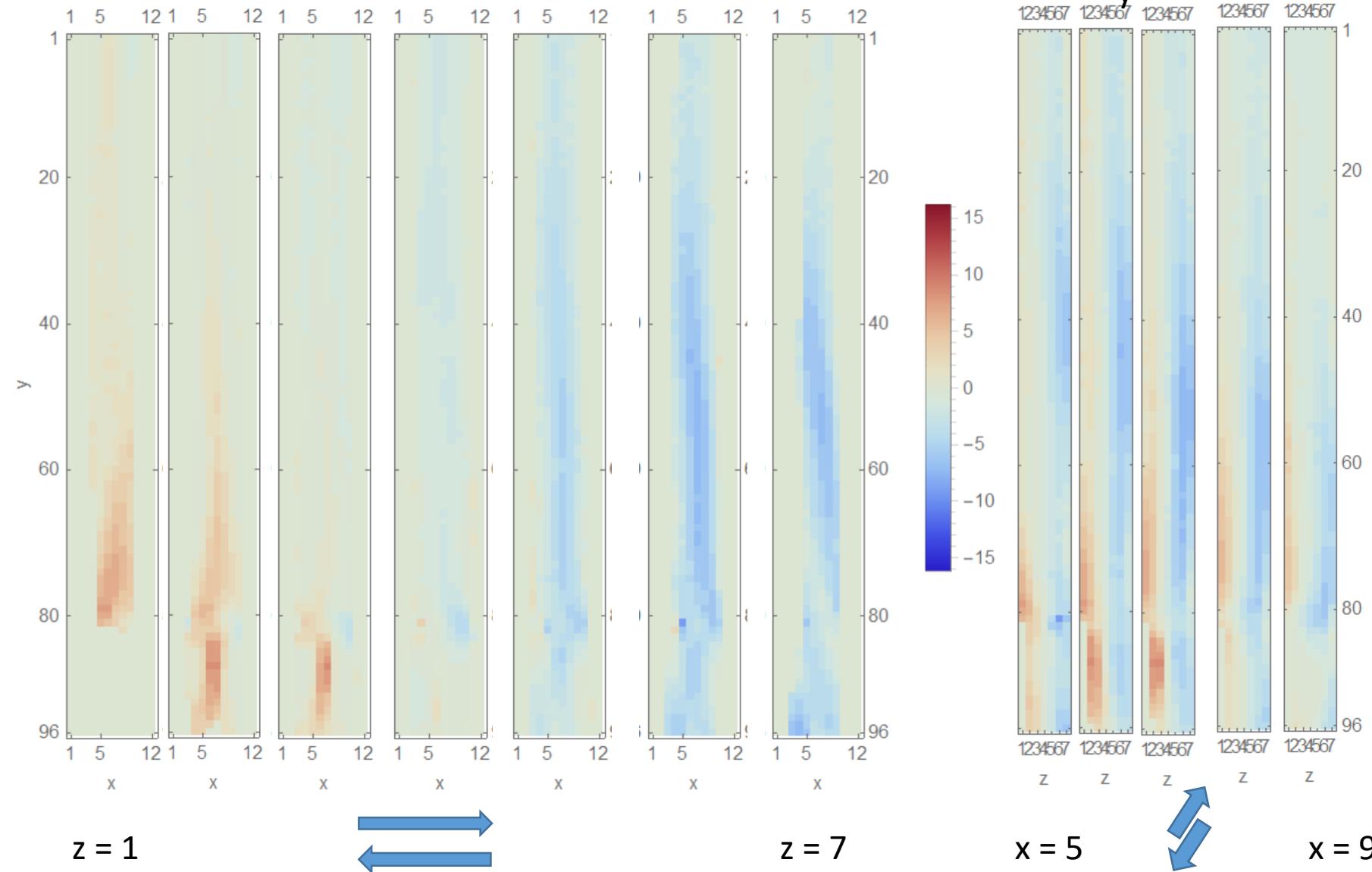
Matrix 96×96×7



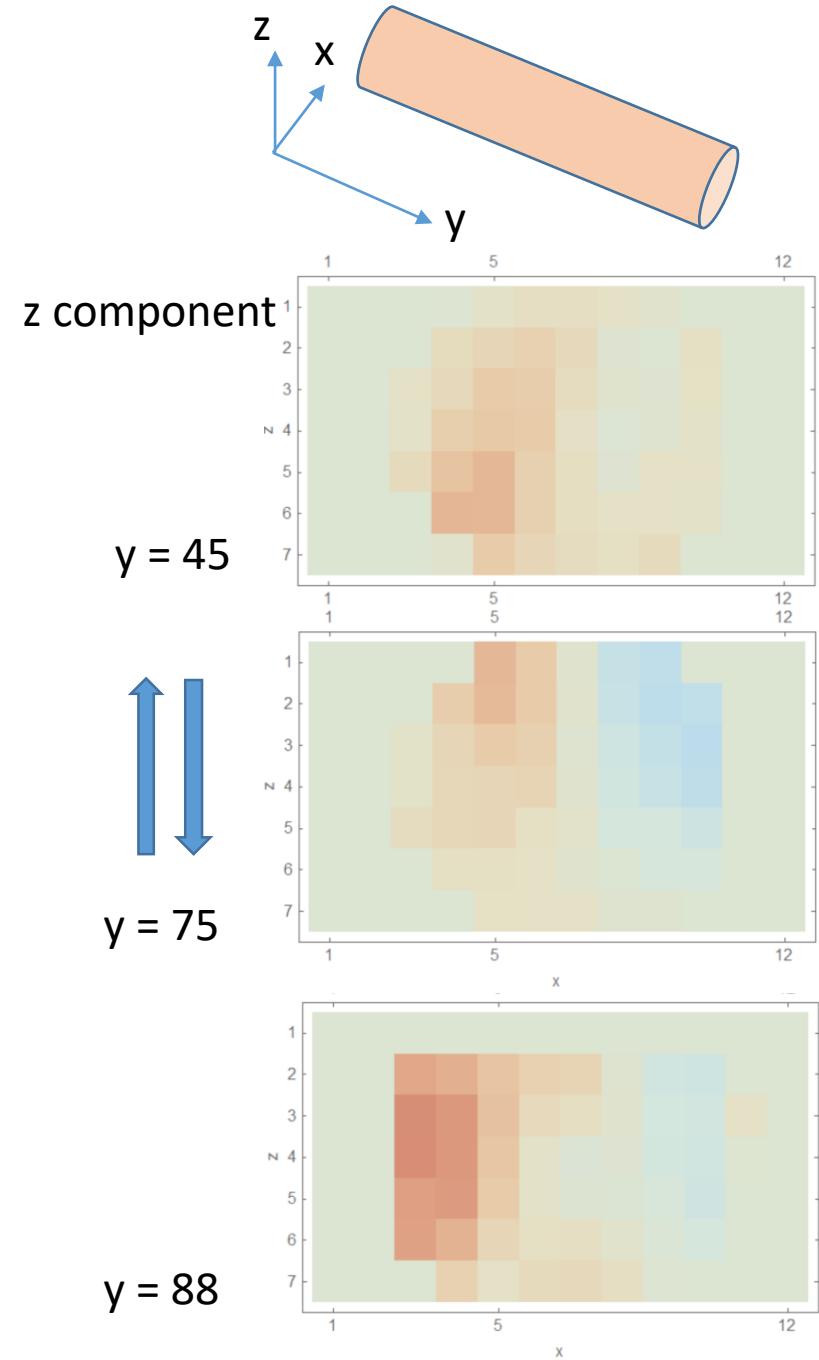
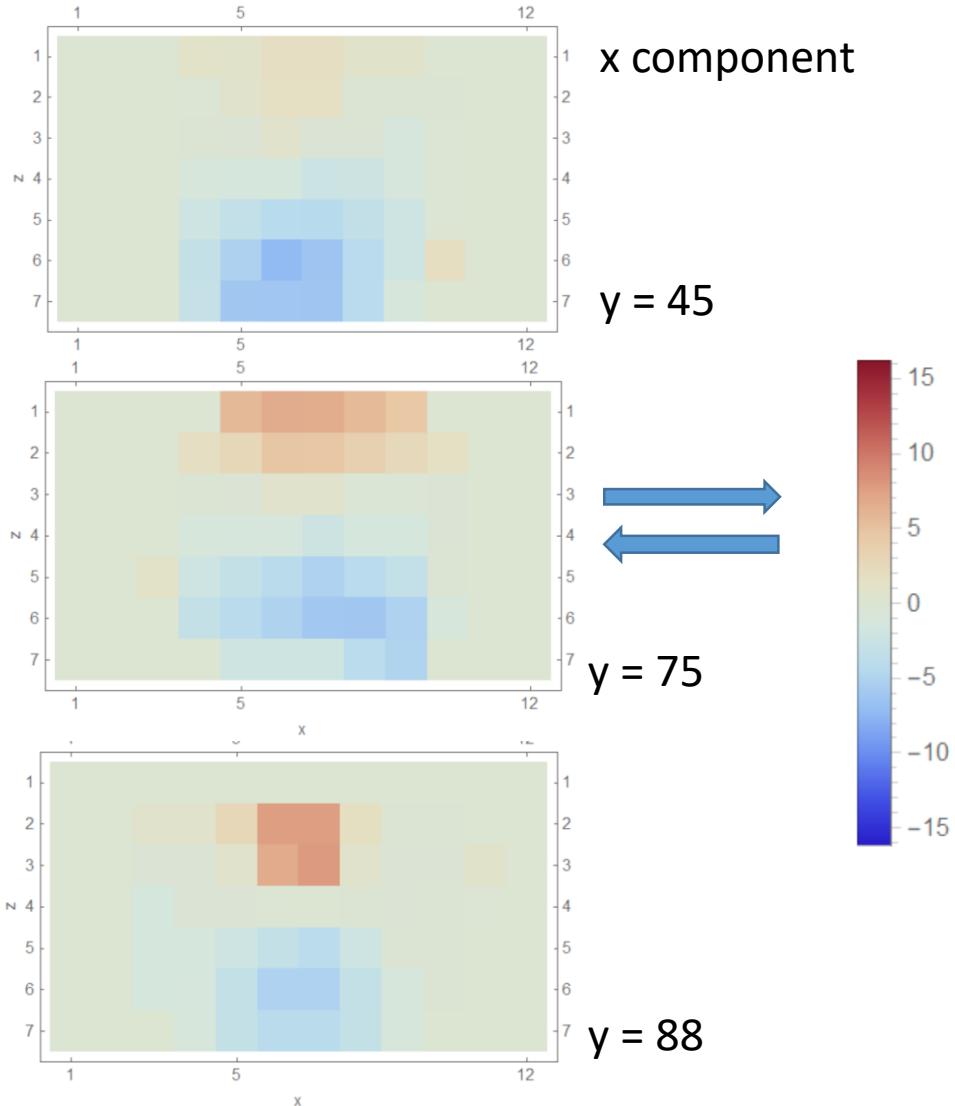
Axial velocity



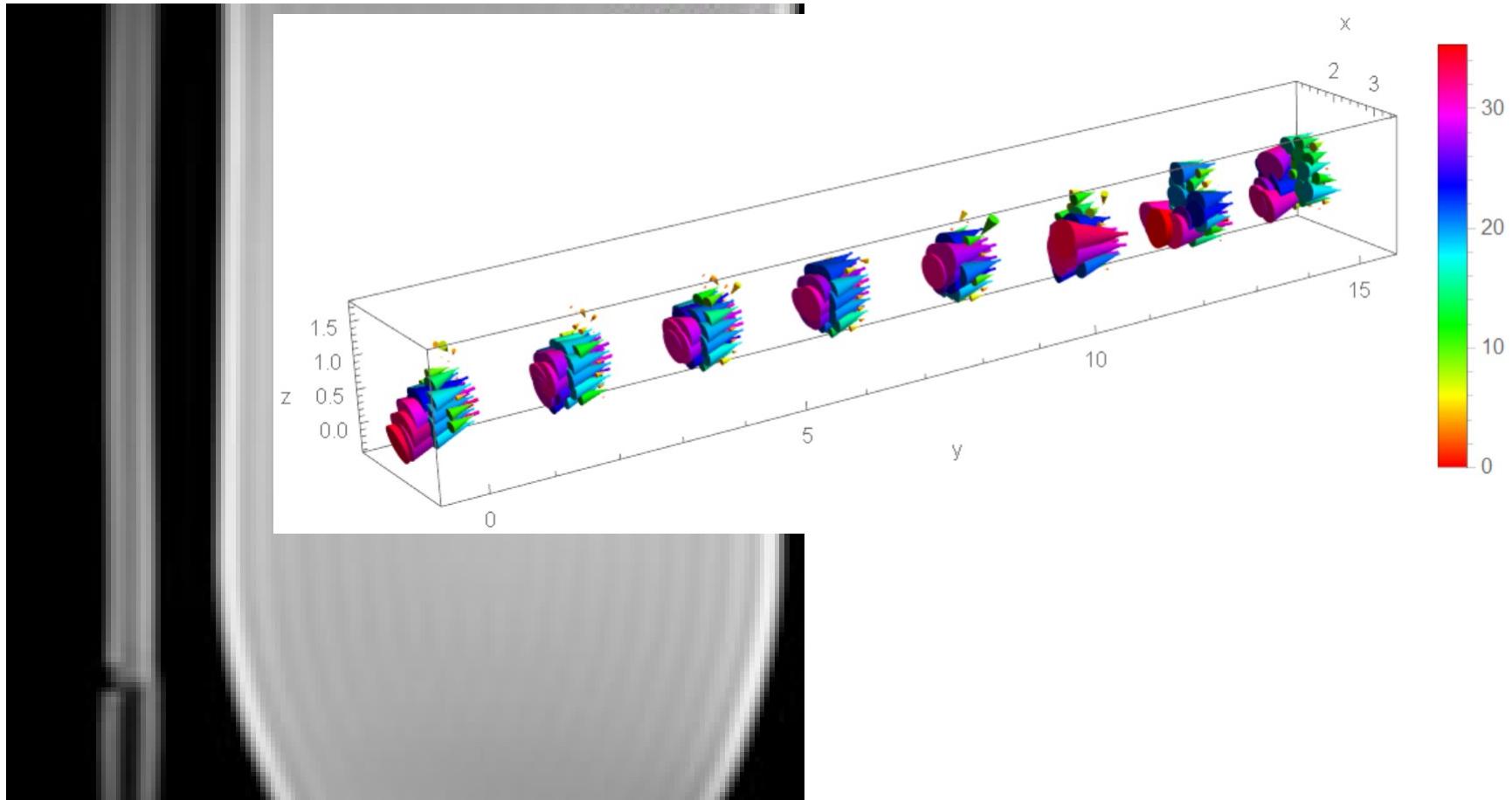
Transversal velocity (x component)



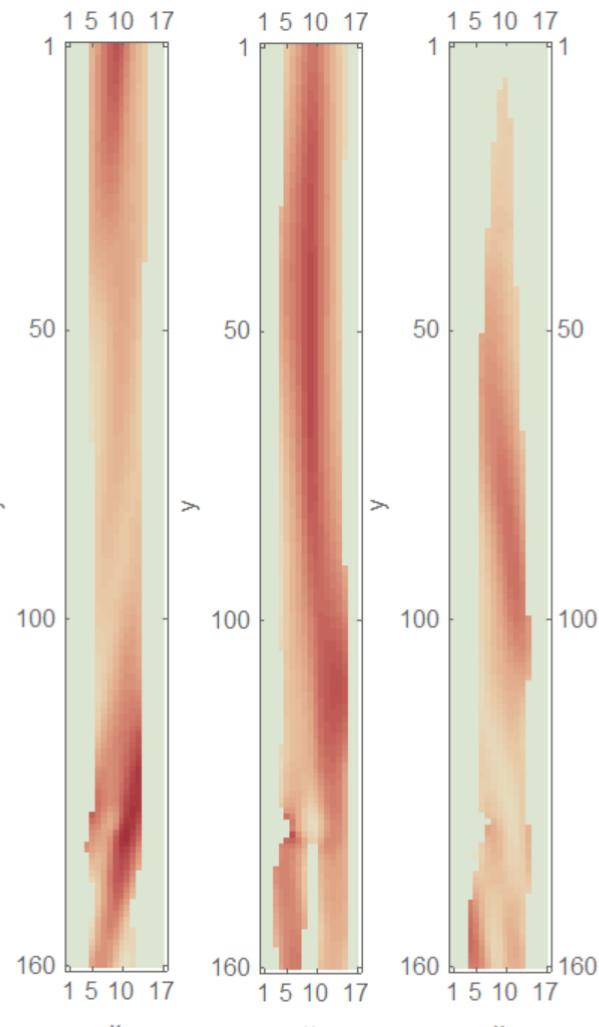
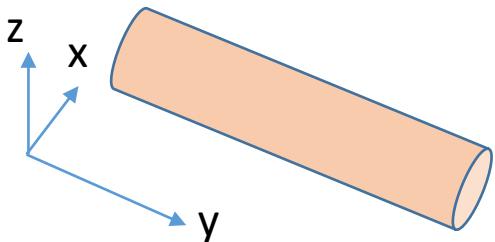
Transversal velocity



Matrix 160×160×11



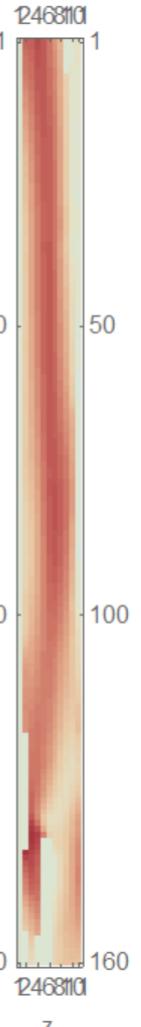
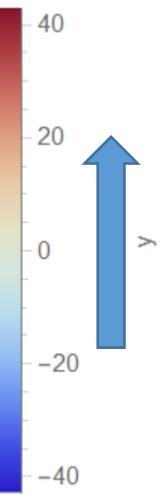
Axial velocity



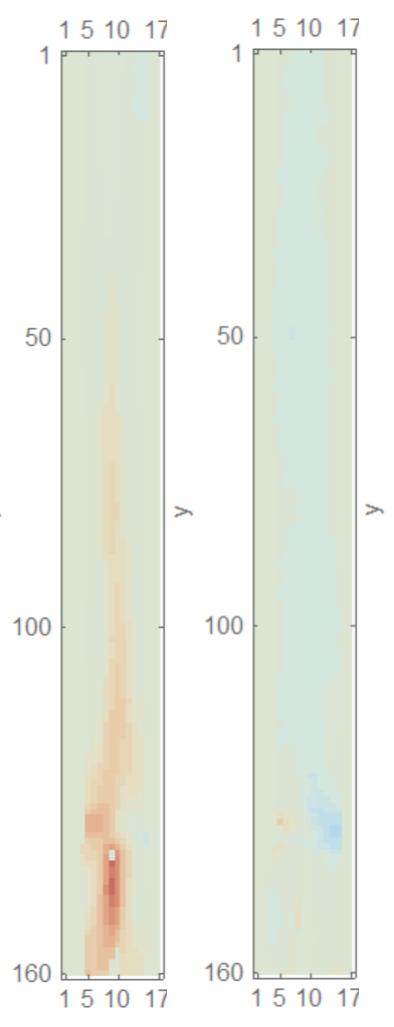
$z = 3$

$z = 6$

$z = 9$



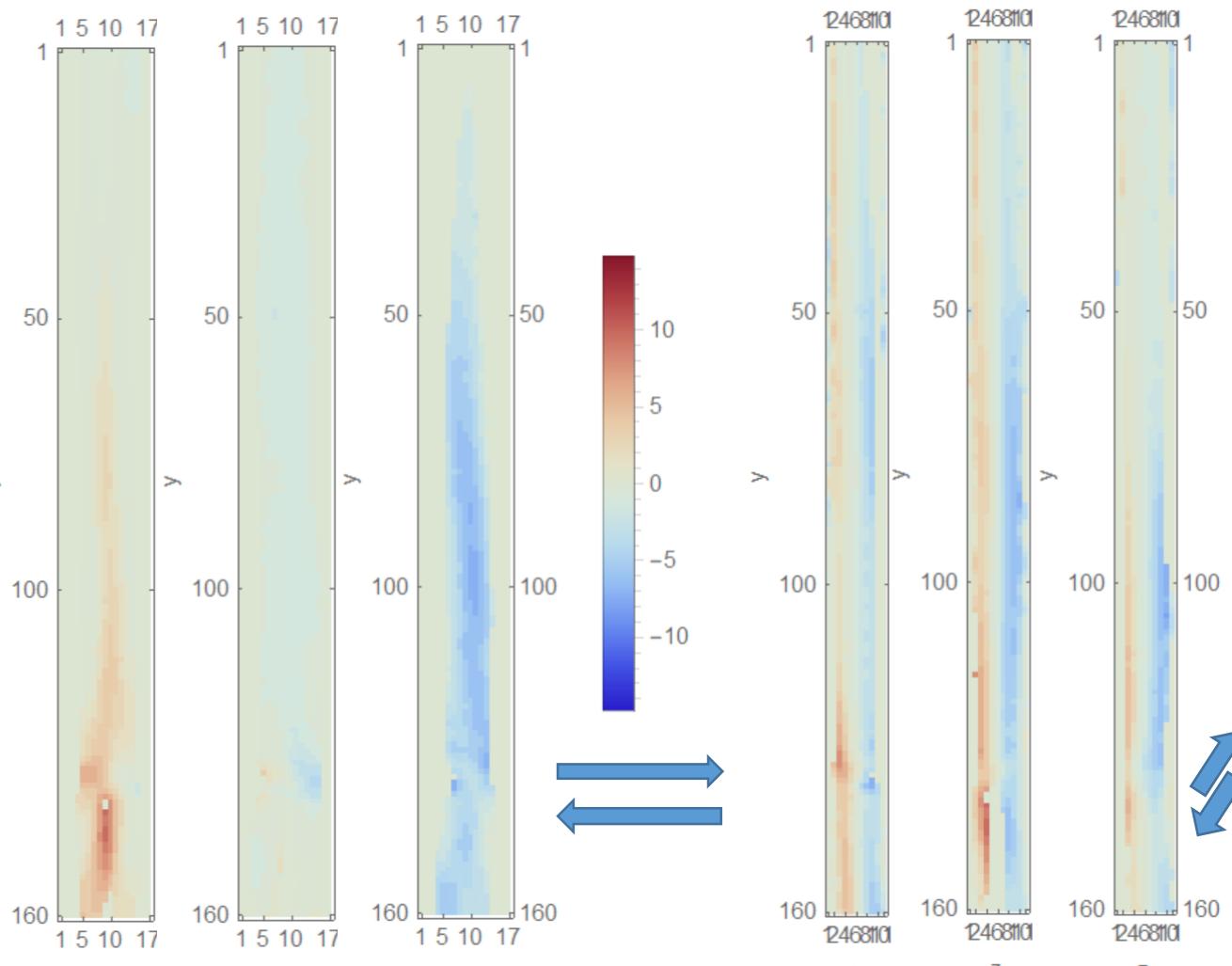
$x = 10$



$x = 4$

$x = 6$

$x = 9$

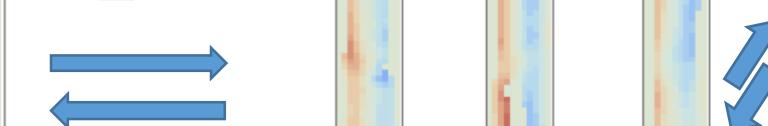


$x = 7$

$x = 9$

$x = 12$

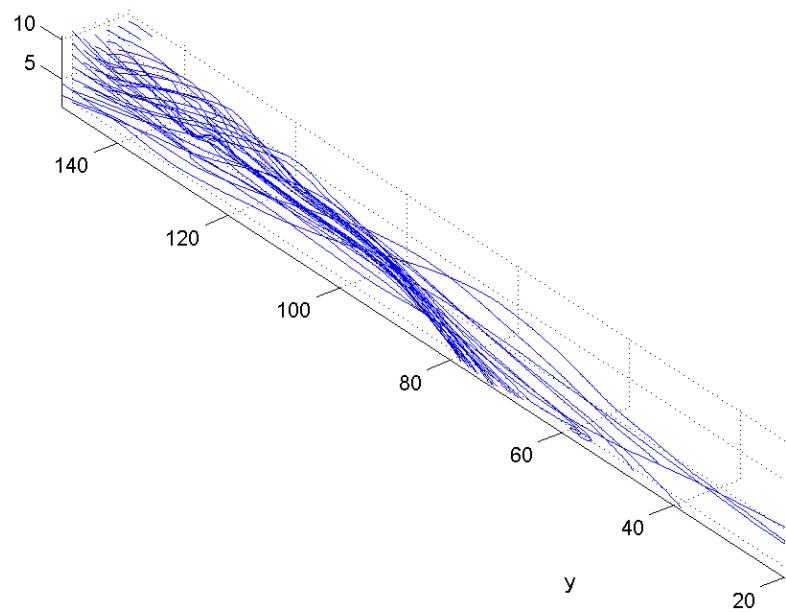
Transversal velocity (x component)



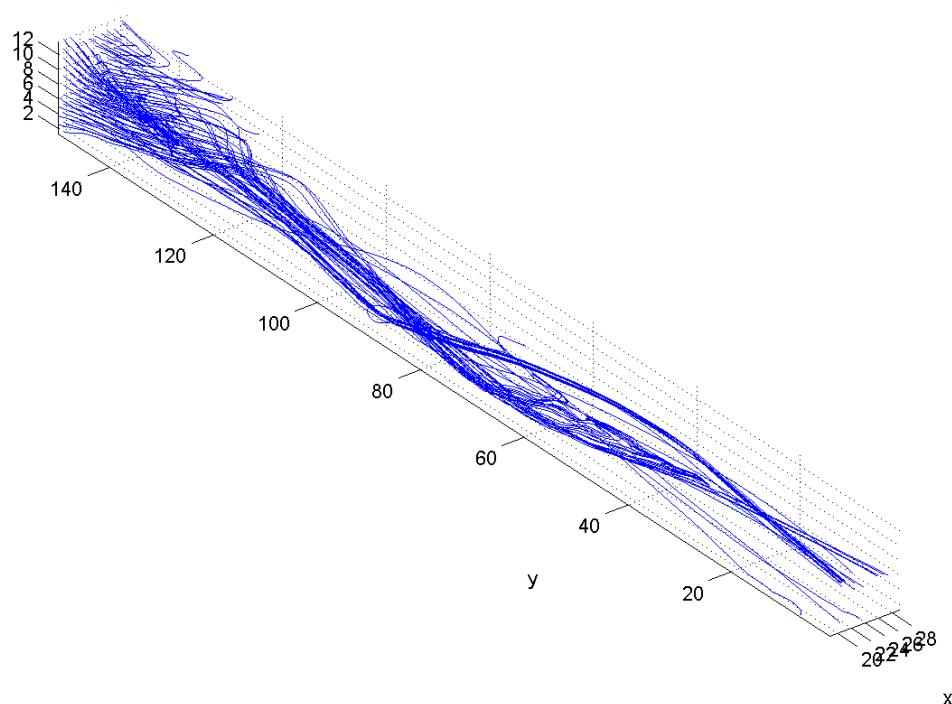
21

Streamlines

$96 \times 96 \times 7$



$160 \times 160 \times 11$

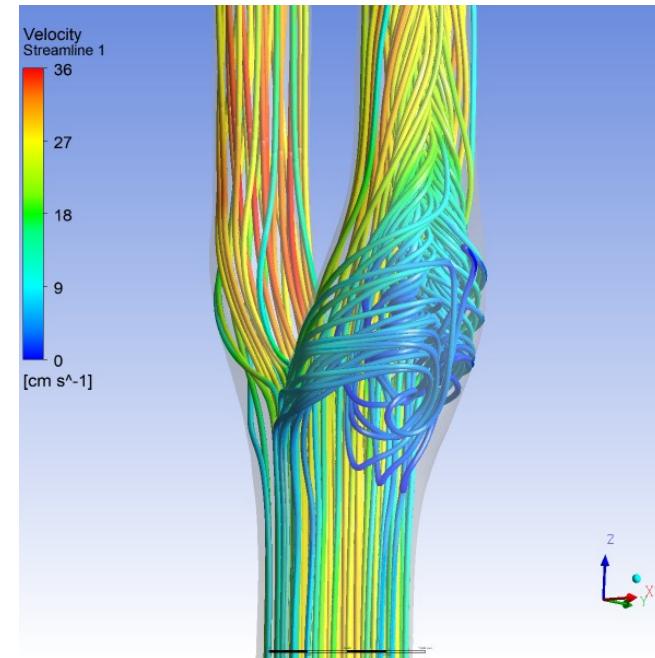
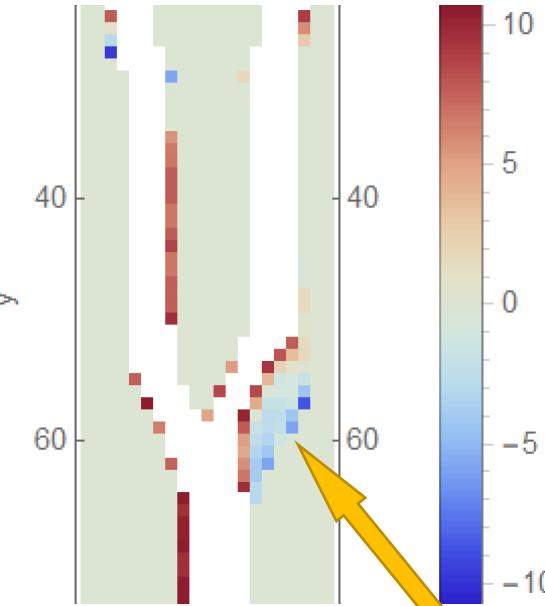
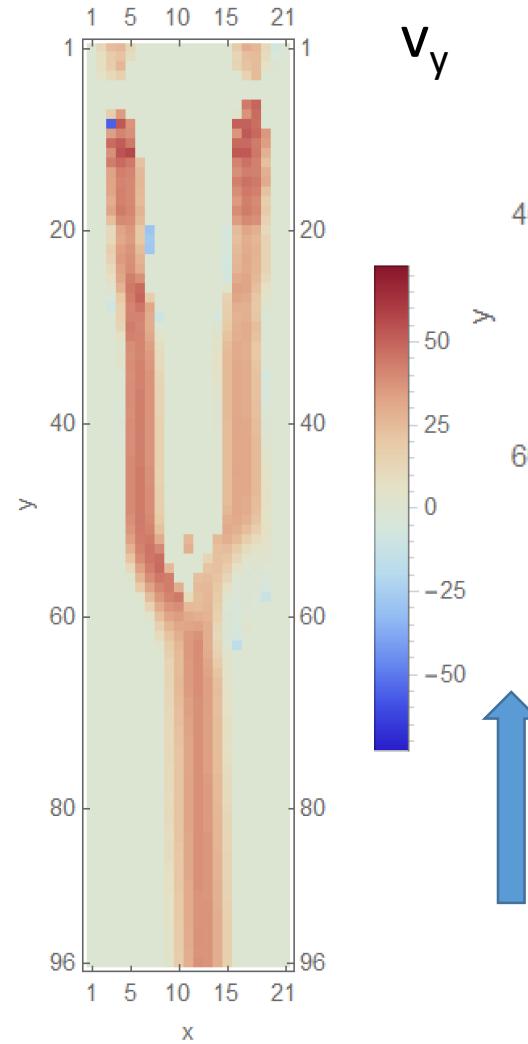


CCA bifurcation

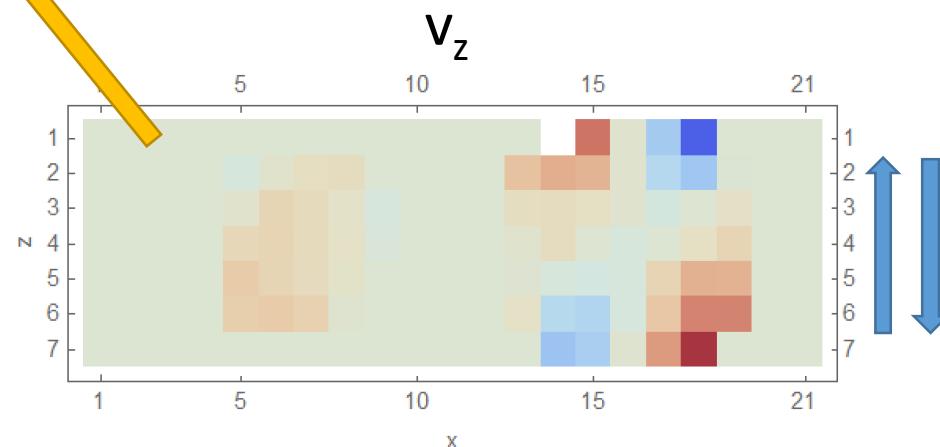


3D matrix	Time steps	Voxel, mm ³	Domain, mm ³	Files
96×96×7	20	1.56×1.56×1.5	150×150×10.5	4 × 280

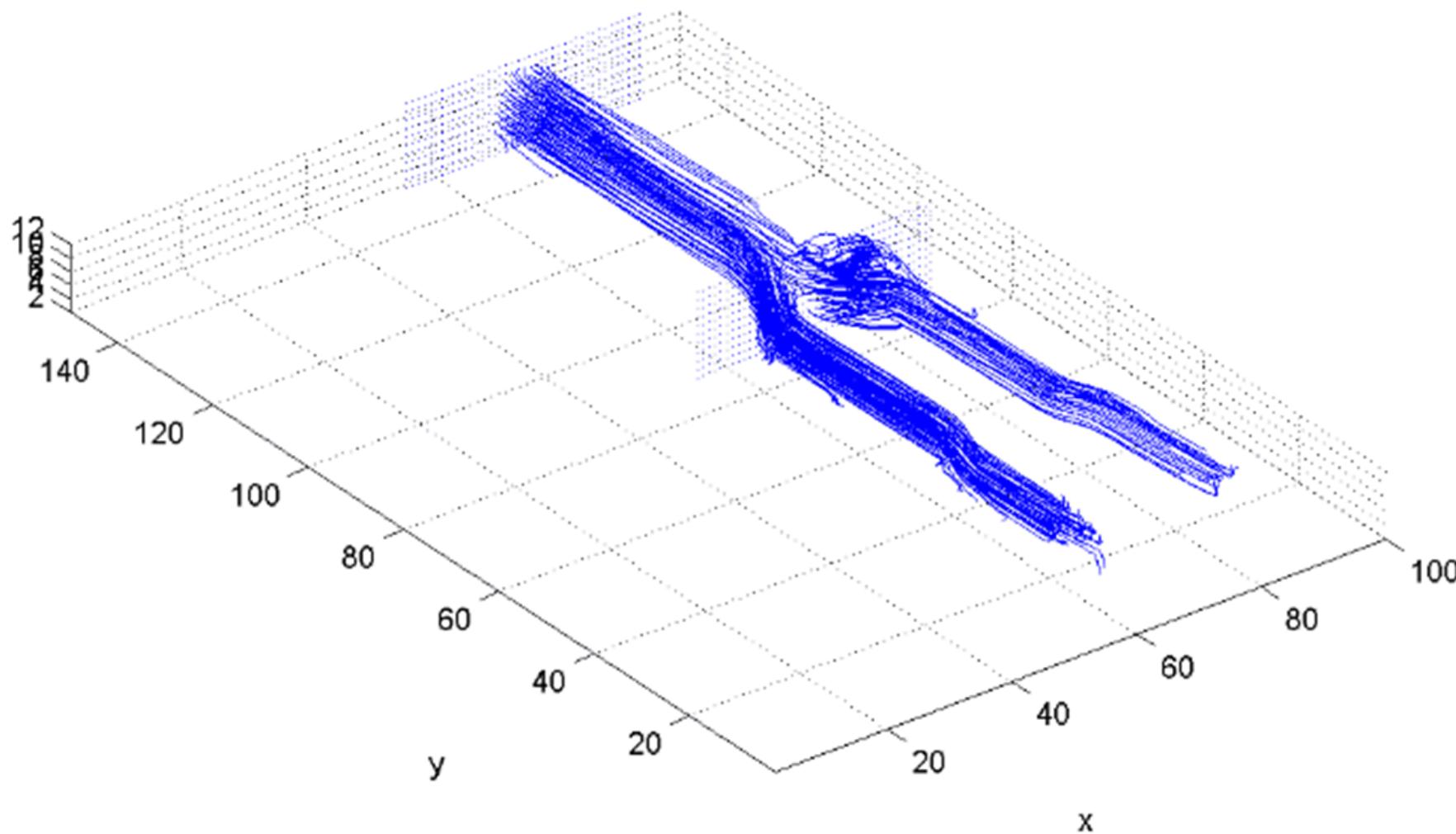
Velocity field



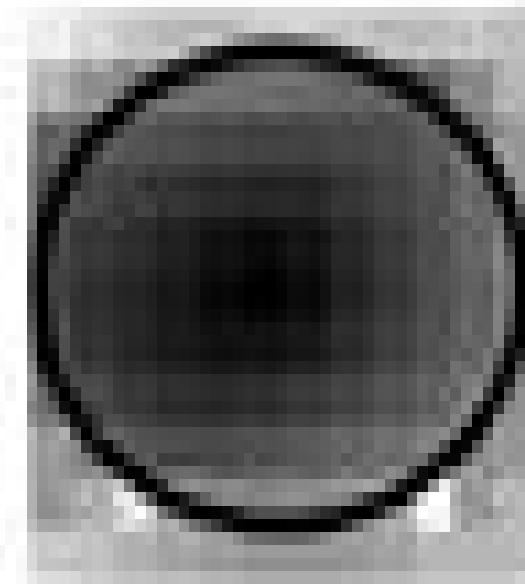
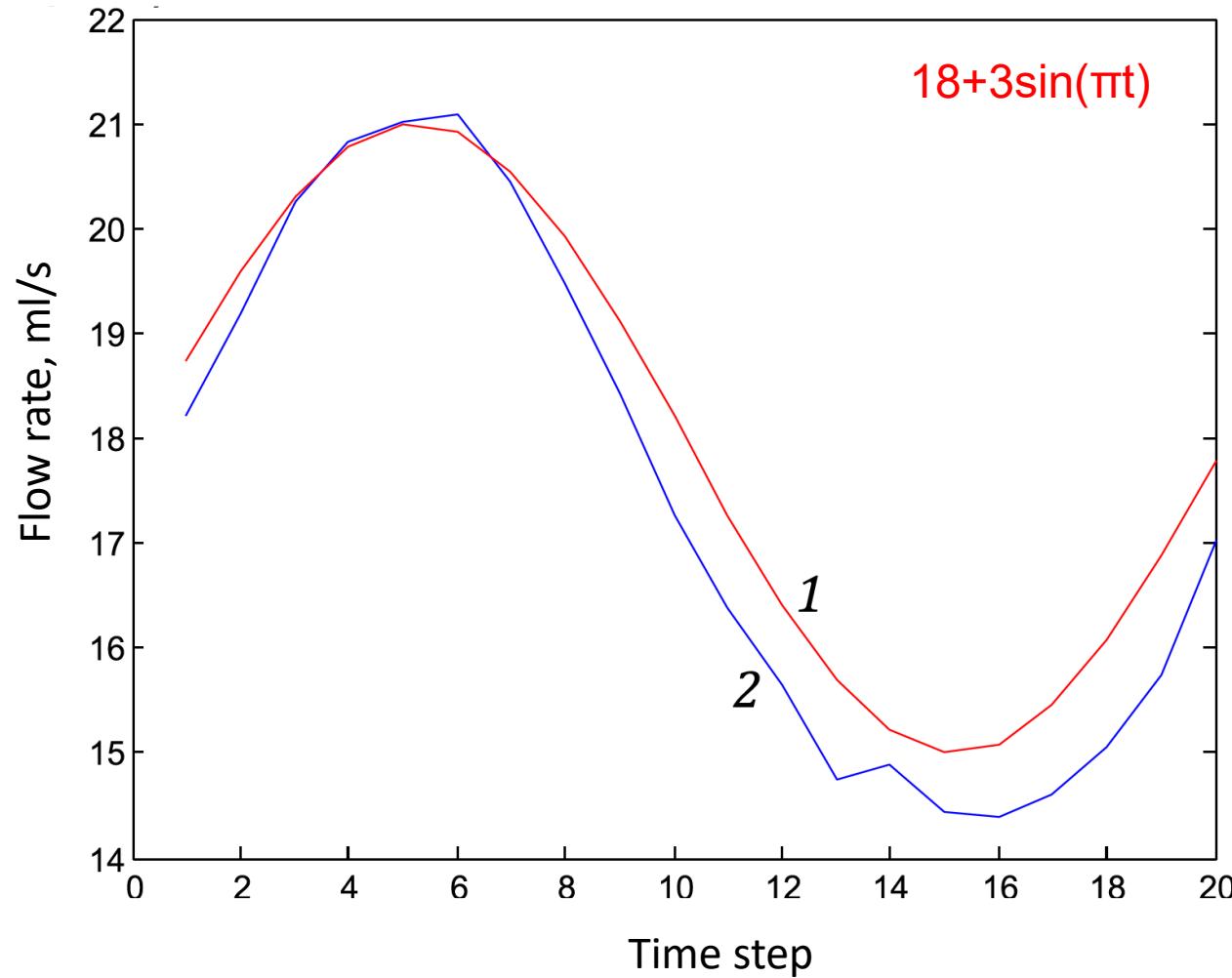
CFX simulation



Streamlines



Flow rate in tube



Tube cross-section

Patients and volunteers

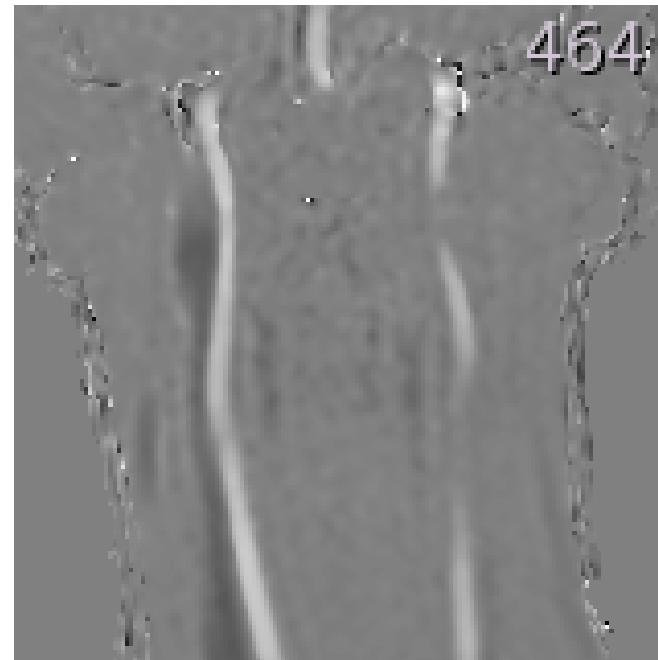
	Patient	ROI	Cross-Section
1	GTS [F, 24 y/o]	BA	Transverse, coronal
2	KMY [M, 39 y/o]	BA, CCA	Transverse, sagittal
3	CTE [F, 33 y/o]	BA	Transverse
4	YGS [F, 24 y/o]	CCA+VA	Coronal
5	LAI [F, 22 y/o]	CCA+VA	Coronal
6	KYO [F, 23 y/o]	CCA+VA	Coronal

LAI [F, 22 y/o]

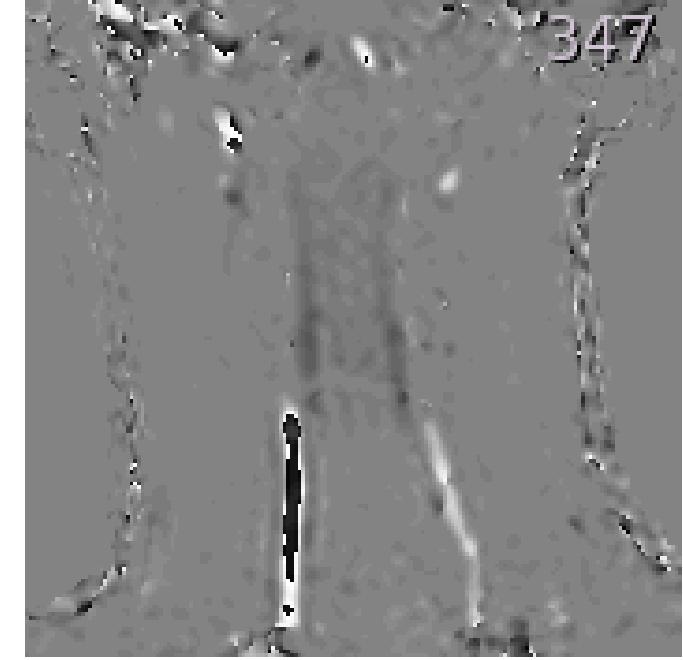
Density



High velocity

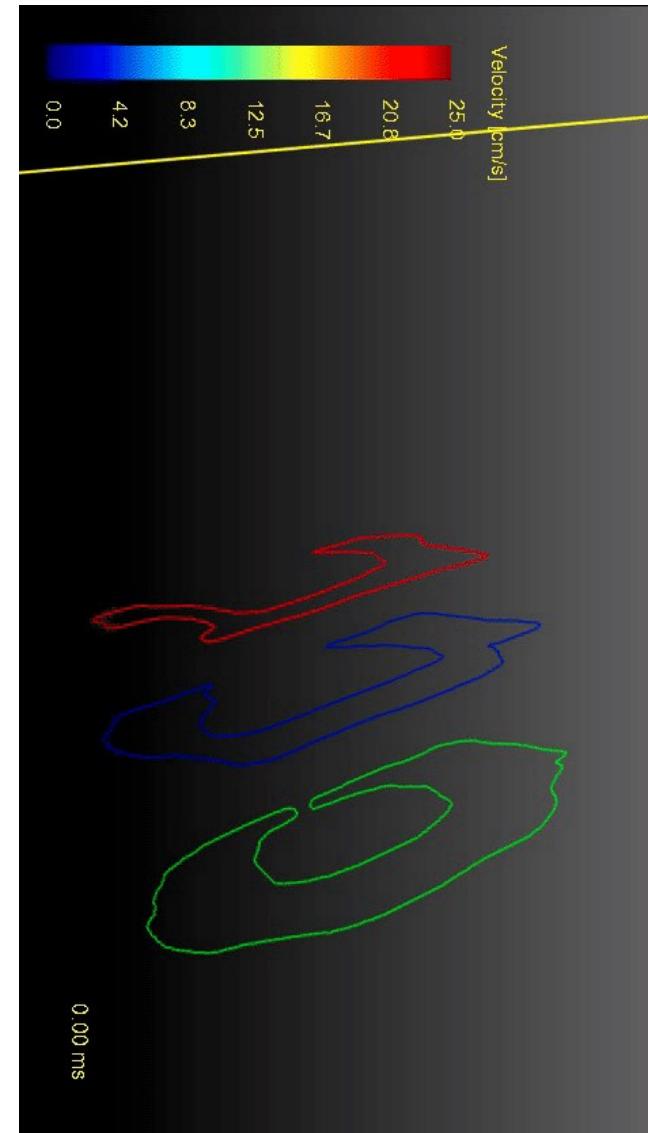


Low velocity



Resolution	Time steps	Voxel size, mm ³	ROI size, mm ³	Max velocity
$160 \times 160 \times 14$	20	$0.94 \times 0.94 \times 1.25$	$150 \times 150 \times 17.5$	100
$176 \times 176 \times 14$	20	$0.86 \times 0.86 \times 1.35$	$152 \times 152 \times 18.9$	18

LAI [F, 22 y/o]



Conclusion

- Possibility to study non-stationary three-dimensional structure of the blood flow with magnetic resonance imaging is shown.
- This allows one to estimate not only volumetric flow rate and linear velocity but also secondary (rotational) flows.
- The scanning protocol is planned to be used in medical examinations for studying the blood and cerebrospinal fluid flow structure and its influence on the functioning of the circulation system and on the development and growth of the pathologies.