

Метод подбора параметров для пациент ориентированного моделирования кровотока

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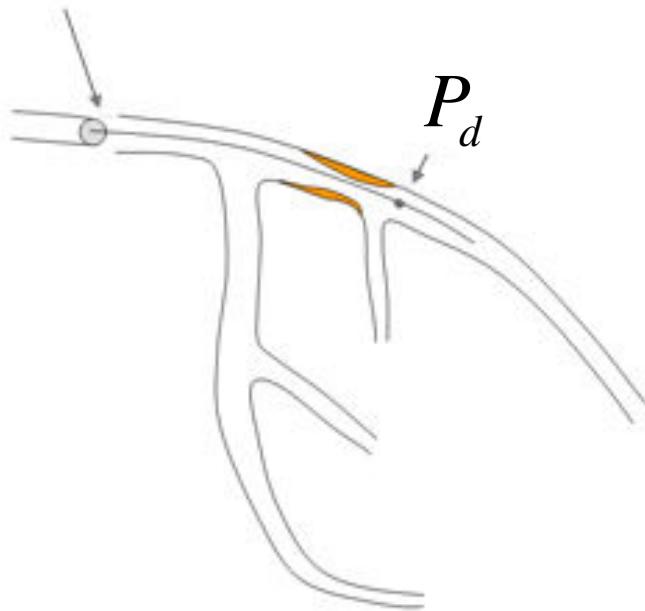


Fractional flow reserve (FFR)



P_{aort}

Vasodilatation



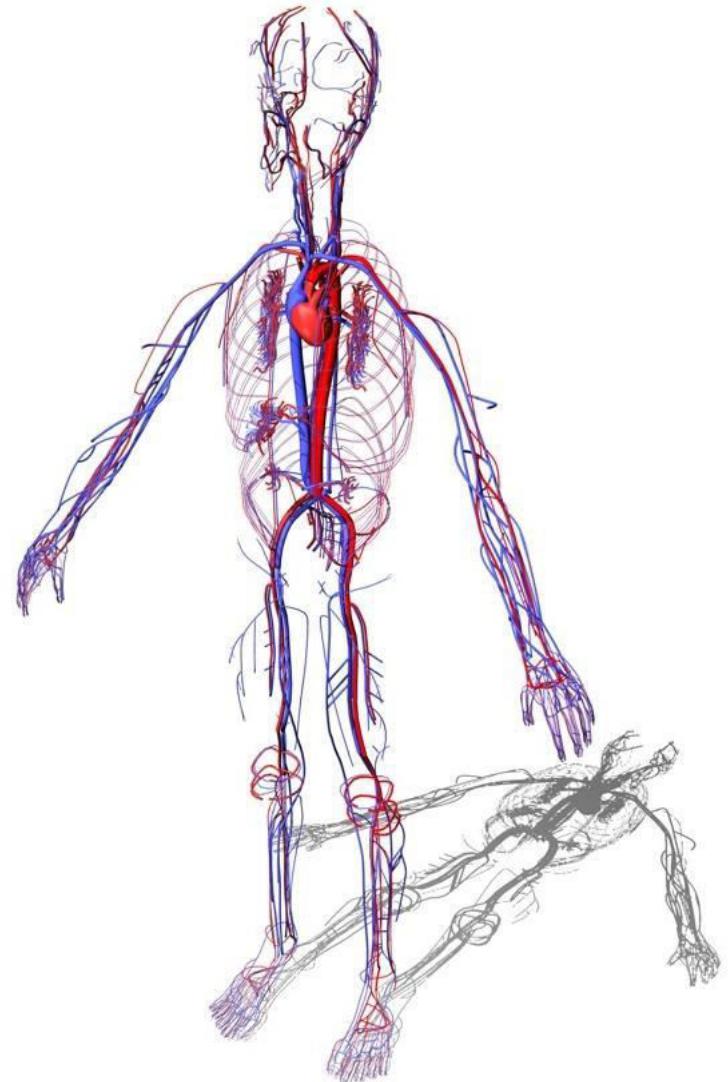
$$FFR = \frac{\text{pressure distal to the lesion } (P_d)}{\text{aortic pressure } (P_{aort})}$$

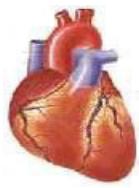
$FFR = 1 \longrightarrow$ healthy subject

$FFR \leq 0.75 \longrightarrow$ surgical treatment



Blood flow model





Model of coronary circulation



$$p_k - p_{veins} = R_k Q_k$$

arteries

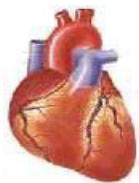
$$\frac{\partial A}{\partial t} + \frac{\partial(uA)}{\partial x} = 0$$

$$\frac{\partial u}{\partial t} + \frac{\partial}{\partial x} \left(\frac{u^2}{2} + \frac{P}{\rho} \right) = f_{fr}$$

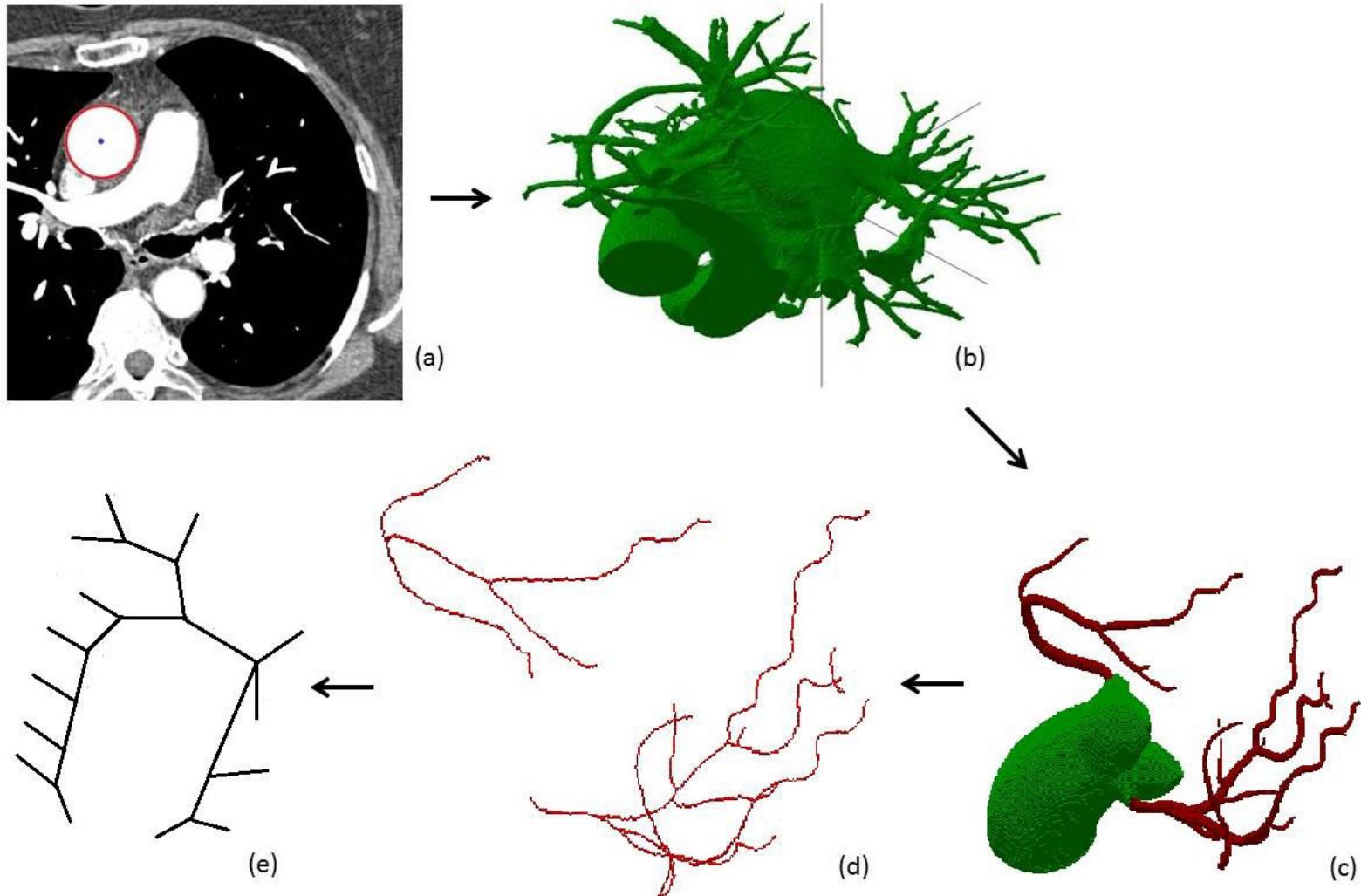
$$u_{in} A_{in} = Q(t)$$

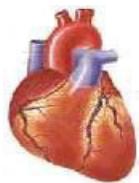
$$p_k + \frac{\rho u_k^2}{2} = p_j + \frac{\rho u_j^2}{2}, \quad \forall j, k$$

$$p_{veins}$$



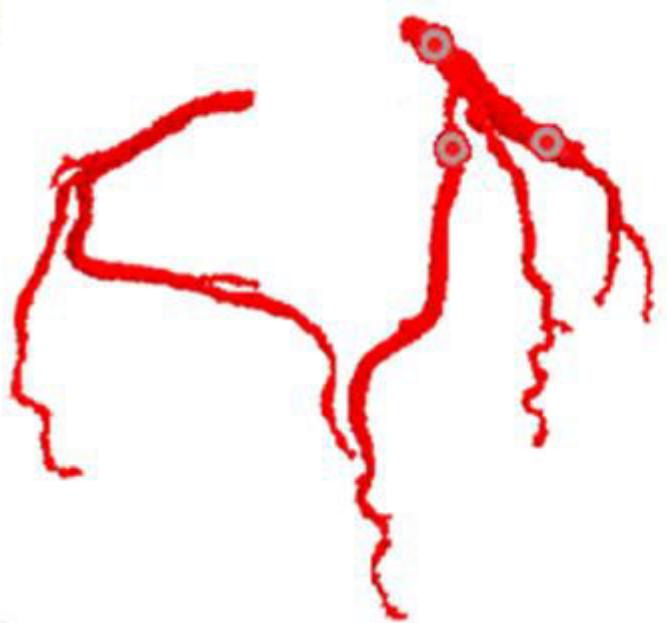
Arterial structure. Patients 1-2.





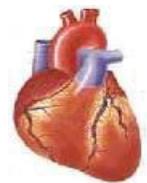
Arterial structure. Patients 1-2.

1

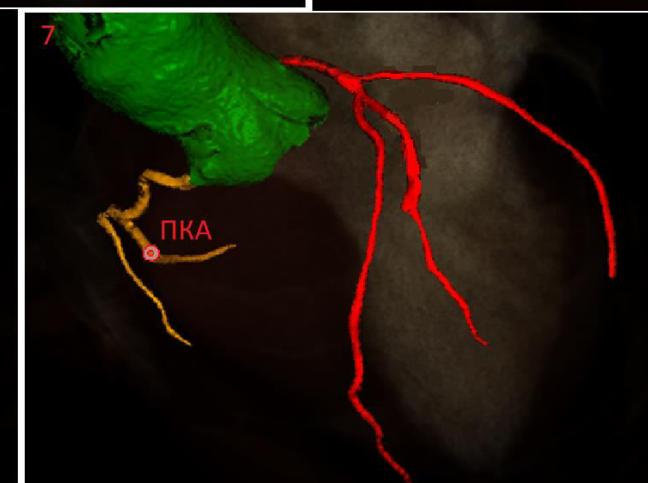
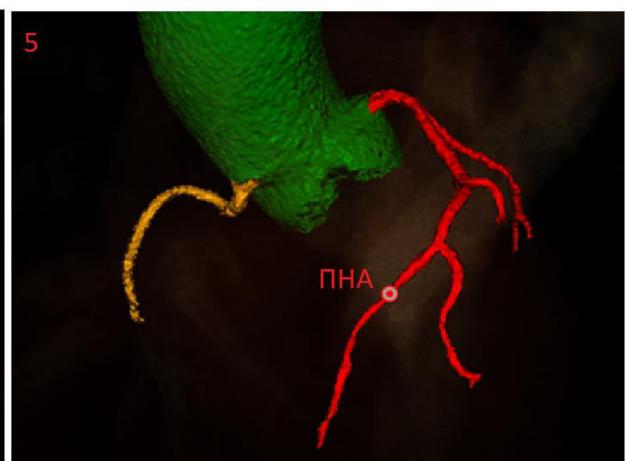
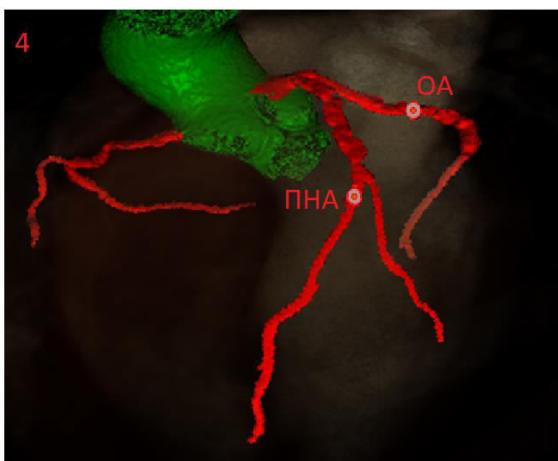


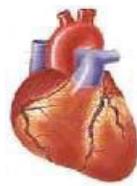
2





Arterial structure. Patients 3-7.





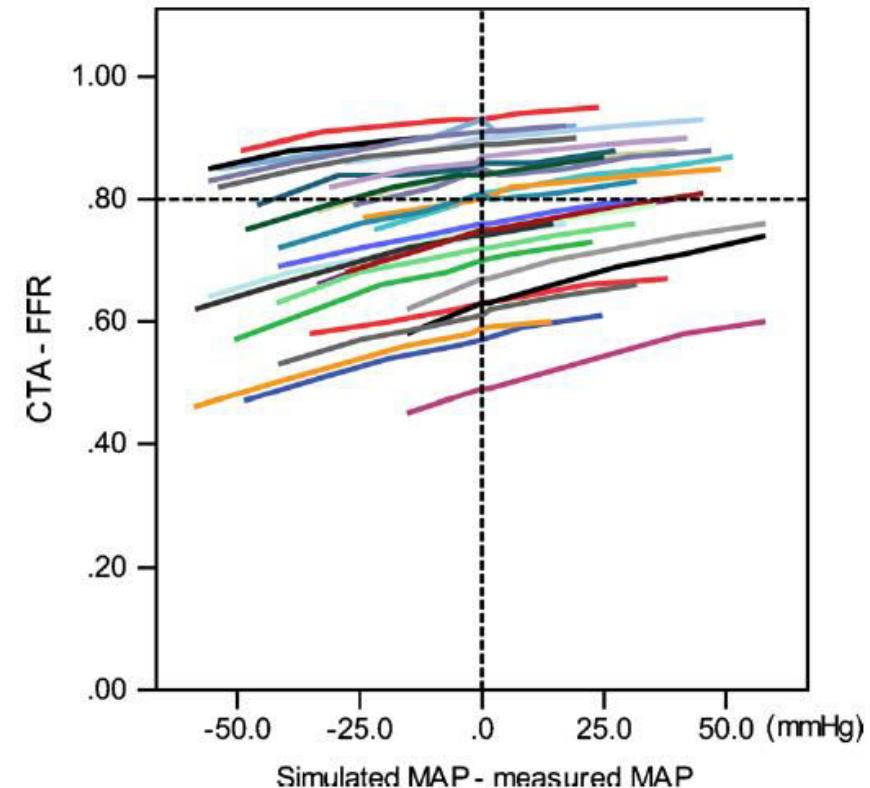
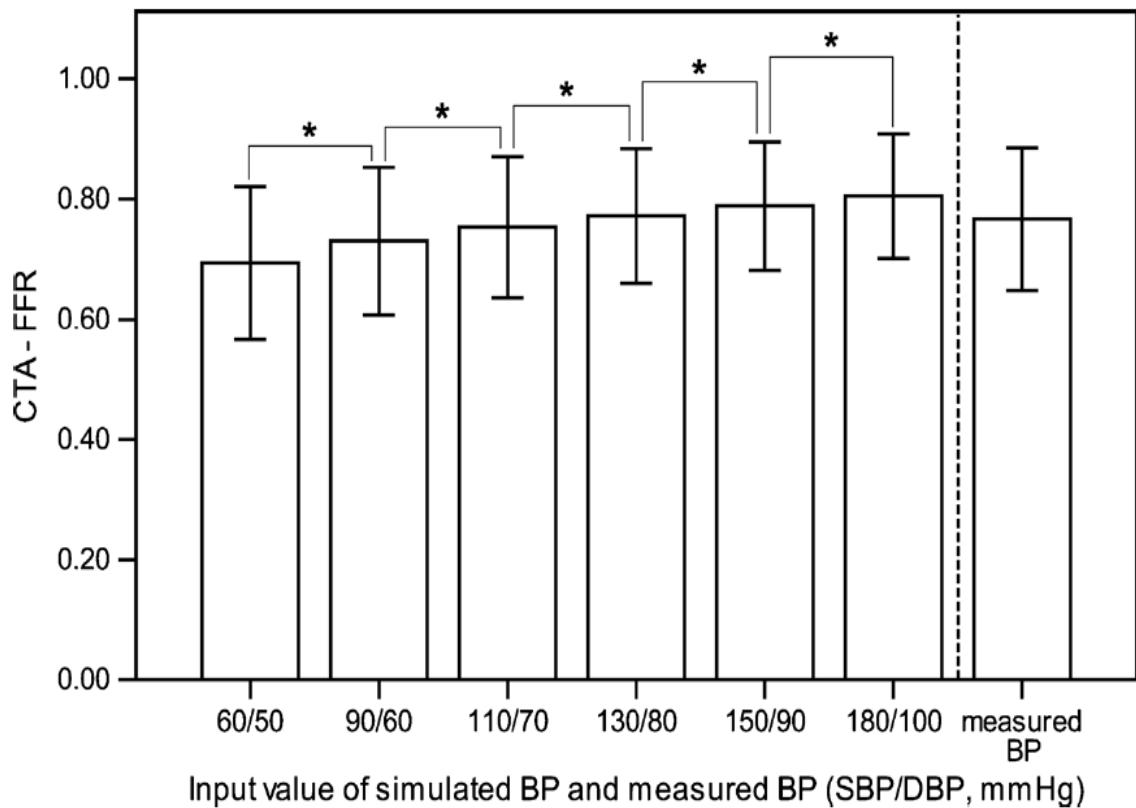
Results



Patient	Vessel	Stenosis	Length, mm	FFR	FFR model	Deviation
1	LAD	50%	40	0.58	0.51	14%
	LCA	55%	2	0.84	0.72	17%
	LCX	80%	10	0.61	0.59	3%
2	LAD	80%	20	0.78	0.74	5%
	RCA	55%	2	0.87	0.93	-5%
3	RCA	70%	20	0.77	0.81	-5%
4	RCA	60%	40	0.57	0.6	-5%
	LCX	50%	10	0.97	0.88	14%
5	LAD	50%	10	0.86	0.91	-5%
6	LCX	50%	10	0.83	0.89	-7%
	RCA	50%	10	0.93	0.91	2%
7	RCA	50%	3	0.89	0.85	5%



Blood pressure and FFR





Parameters estimation



Parameters
(stroke volume,
elasticity,
resistance,..)



Blood flow model



output values
(systolic BP,
diastolic BP)



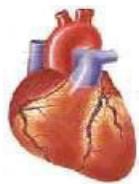
Parameters estimation. Learning



1. “Base” model $M(\vec{p}) = \vec{u}$

$$M(\vec{p} + \Delta\vec{p}_k) = \vec{u} + \Delta\vec{u}_k$$

$$\Delta\vec{p}_k \longrightarrow \Delta\vec{u}_k$$

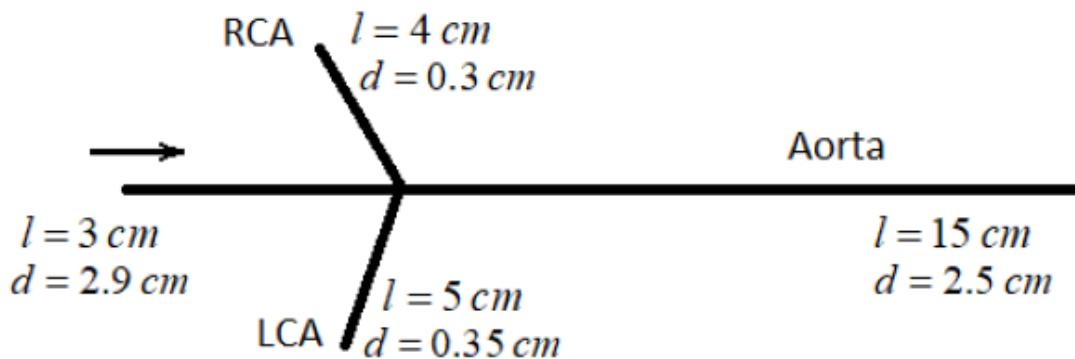


Parameters estimation. Learning

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$$\Delta\vec{p}_k \longrightarrow \Delta\vec{u}_k$$



$$\vec{p} = \{R_a, c_a, SV\}^T$$

$$\vec{u} = \{P_s, P_d\}^T$$



Parameters estimation



2. Current model $\tilde{M}(\vec{p})$

$$\Delta \vec{p}_k \longrightarrow \Delta \vec{u}_k$$



Parameters estimation

2. Current model $\tilde{M}(\vec{p})$

$$\Delta \vec{p}_k \longrightarrow \Delta \vec{u}_k$$

$$\Delta \vec{p} = \sum_{k=1}^K x_k \Delta \vec{p}_k \quad \Delta \vec{u} = \vec{u}^* - \tilde{M}(\vec{p})$$

$$\tilde{M}(\vec{p} + \Delta \vec{p}) - \tilde{M}(\vec{p}) = \Delta \vec{u}$$

$$\Delta \vec{u} = \sum_{k=1}^K x_k \Delta \vec{u}_k, \quad x_k^{min} \leq x_k \leq x_k^{max}$$

$$\sum_{k=1}^K x_k^2 \rightarrow min$$



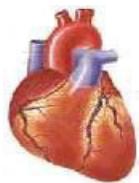
$$\Delta \vec{u} = \sum_{k=1}^K x_k \Delta \vec{u}_k, \quad x_k^{min} \leq x_k \leq x_k^{max} \quad \Delta \vec{u} \in R^M, \quad M < K$$

$$\sum_{k=1}^K x_k^2 \rightarrow min \longrightarrow \sum_{k=1}^{K-M} x_i^2 + \sum_{i=1}^M \left(\left(\sum_{j=1}^{K-M} \alpha_{ij} x_j \right) + \beta_i \right) \rightarrow min$$



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$$x_i, i = K - M + 1 \dots K$$



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$$\vec{x}' = \{x_1, x_2, \dots x_{K-M}\}^T$$

$$\Phi(\vec{x}') = \langle A\vec{x}', \vec{x}' \rangle + 2\langle \vec{b}, \vec{x}' \rangle + c \rightarrow \min, \quad A \geq 0$$



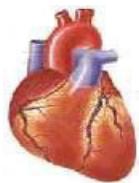
$$\Delta \vec{u} = \sum_{k=1}^K x_k \Delta \vec{u}_k, \quad x_k^{min} \leq x_k \leq x_k^{max} \quad \Delta \vec{u} \in R^M, \quad M < K$$

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$$\vec{x}' = \{x_1, x_2, \dots, x_{K-M}\}^T$$

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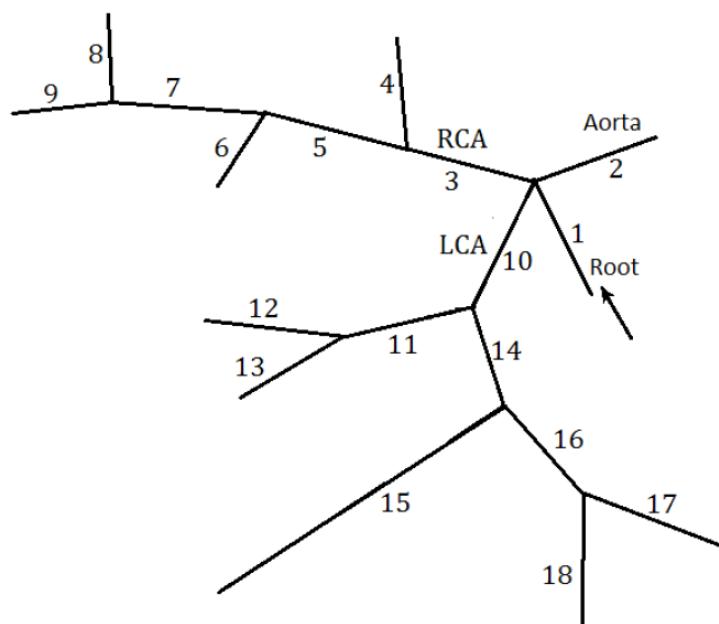
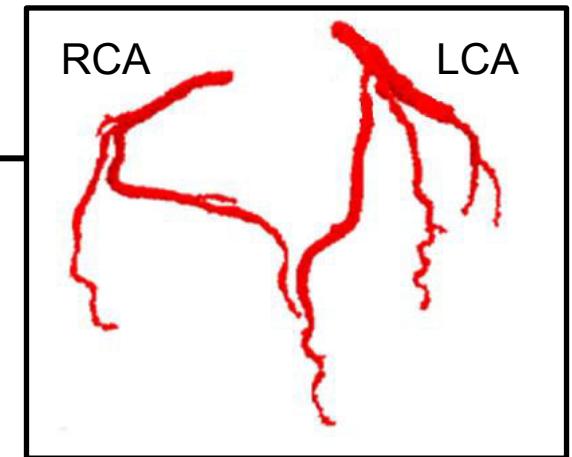
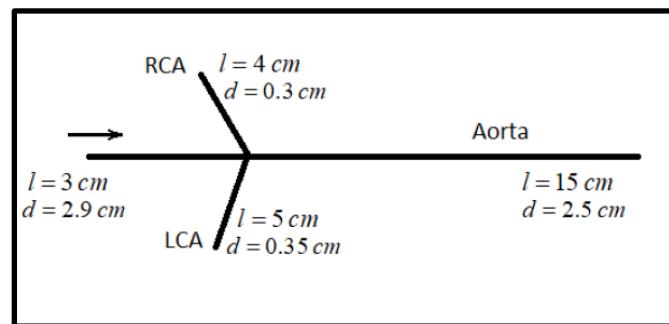
$$\vec{x}'_{\min} : \quad A\vec{x}' + \vec{b} = 0$$



Parameters estimation

2. Current model $\tilde{M}(\vec{p})$

$$\Delta \vec{p}_k \longrightarrow \Delta \vec{u}_k$$

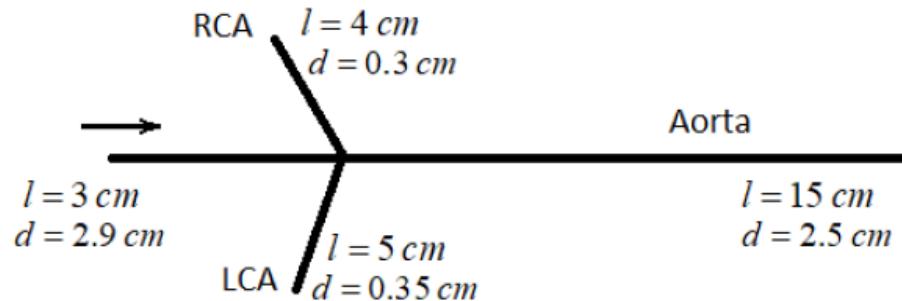




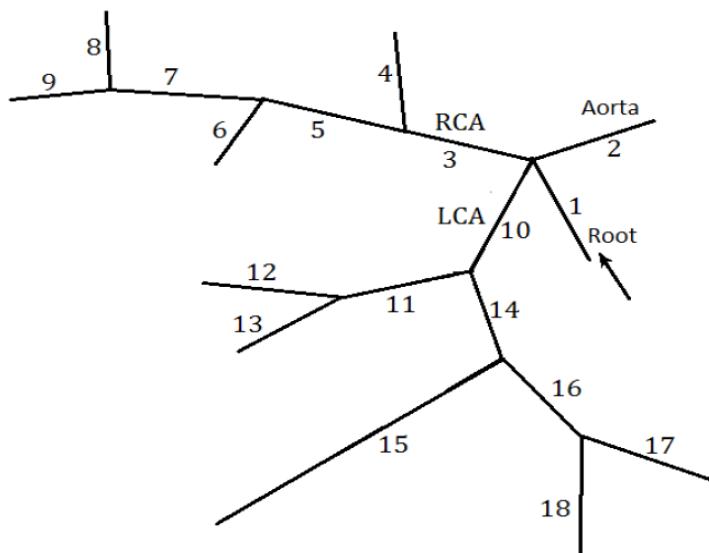
“Base” model and “new” model



“Base” model



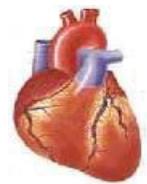
“New” model



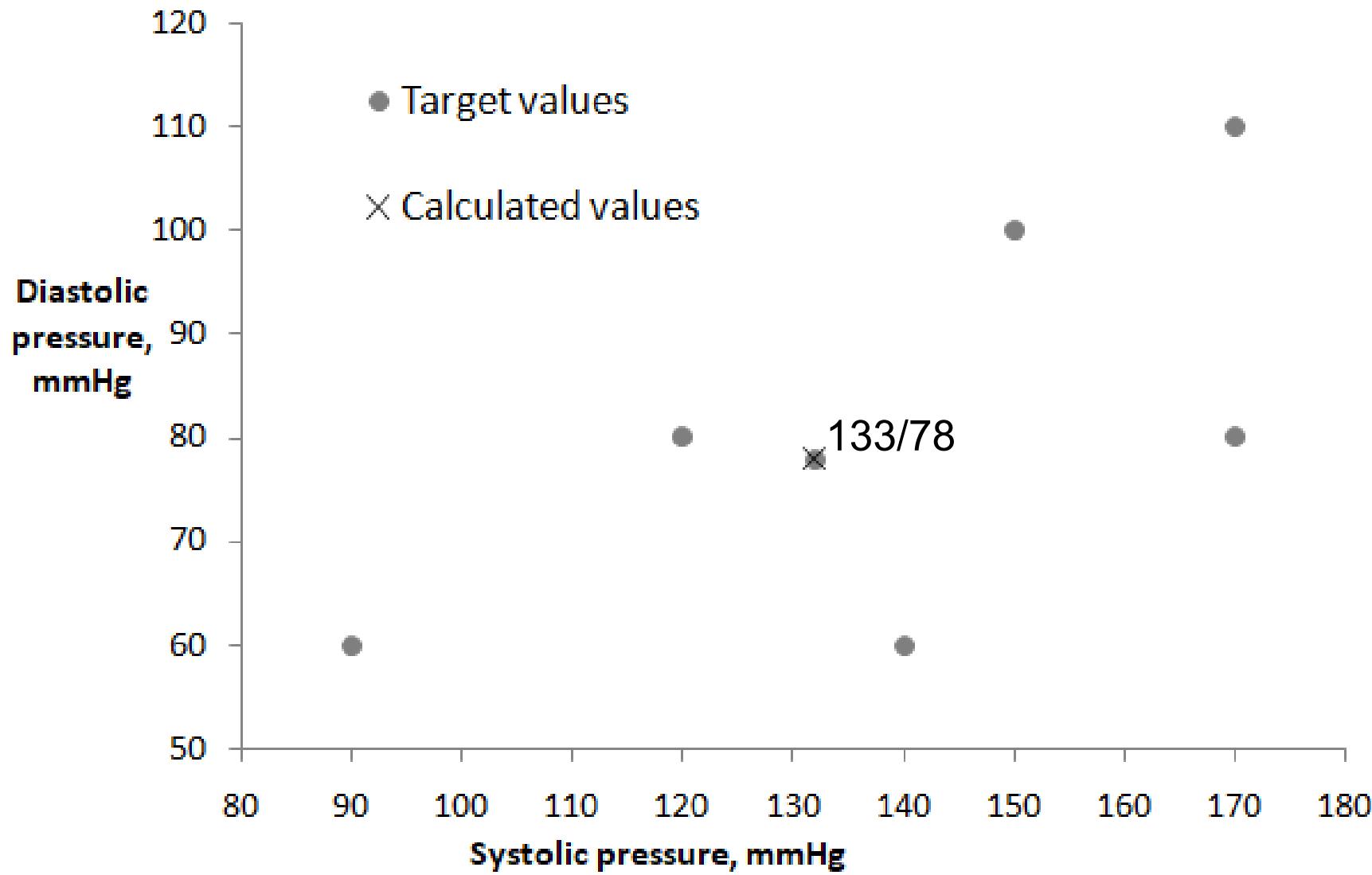
$$\vec{p} = \{R_a, c_a, SV\}^T$$

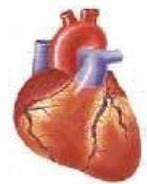
$$\vec{u} = \{P_s, P_d\}^T$$

$$\Delta \vec{p}_k \longrightarrow \Delta \vec{u}_k$$

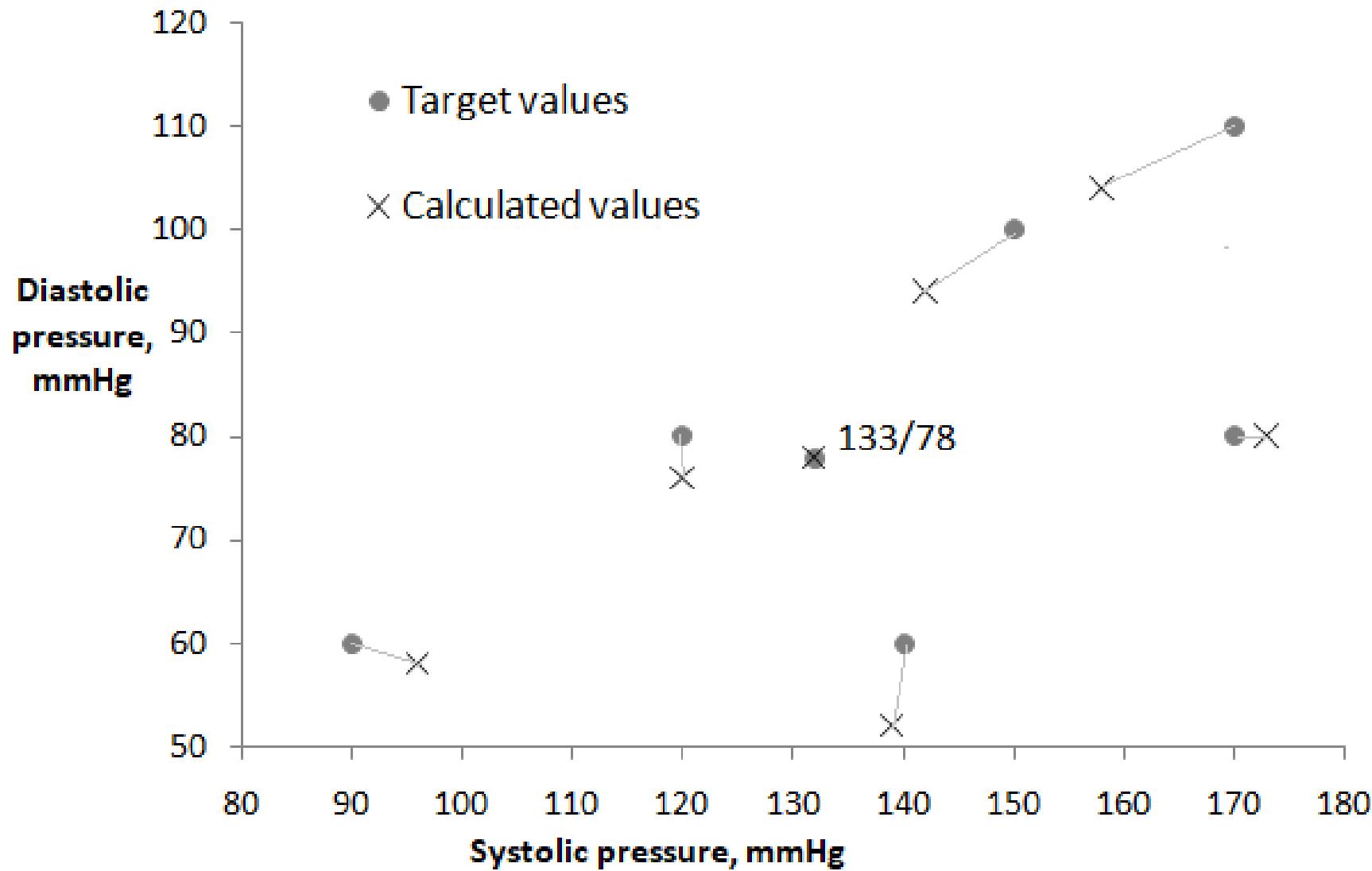


Simulation results





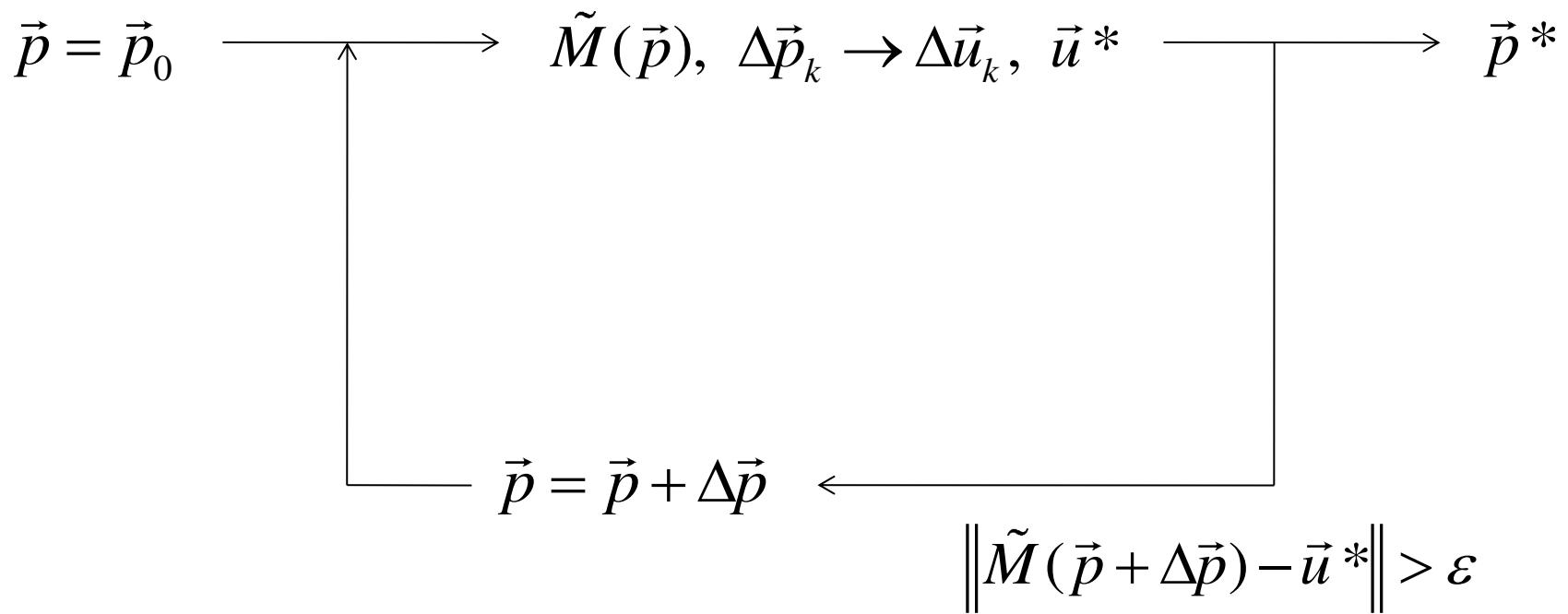
Simulation results

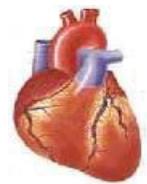


$$\sigma_{\max} = 12 \text{ mmHg}$$

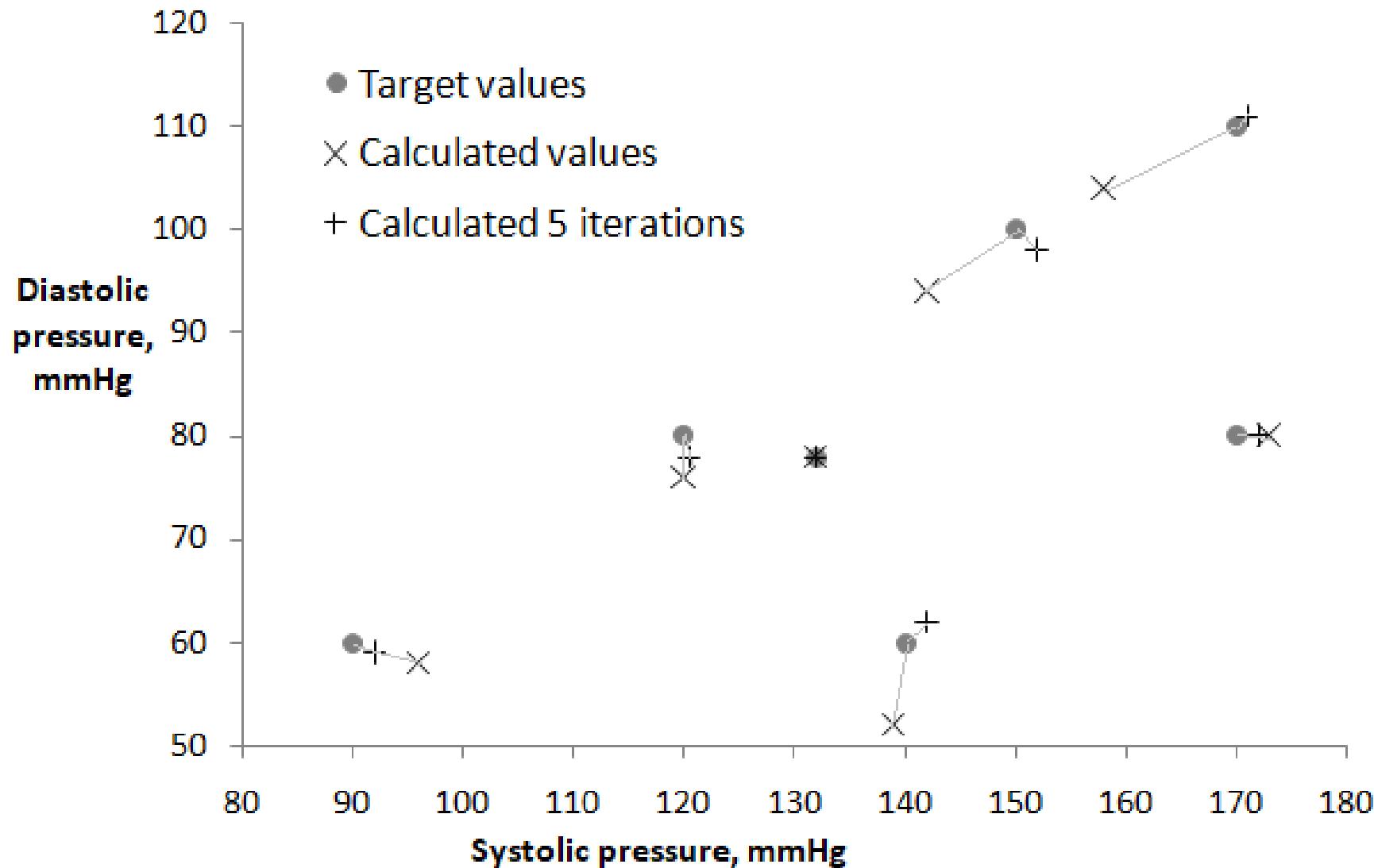


Additional iterations

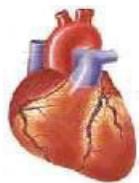




Simulation results



$$\sigma_{\max} = 2 \text{ mmHg}$$



Parameters estimation

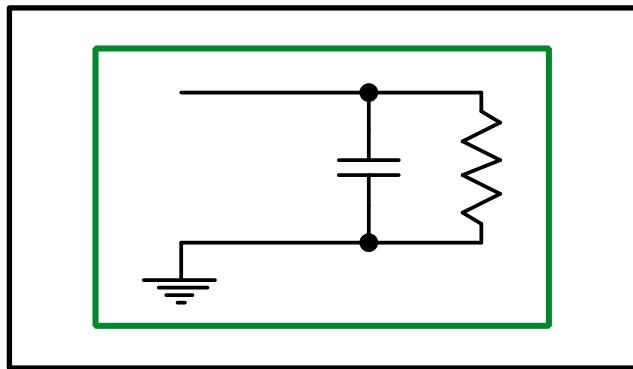
Parameters

$$P_{out}, C, \tau$$

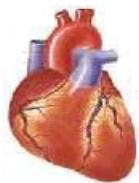
$$\tau = RC$$



0-D: 2-element Windkessel



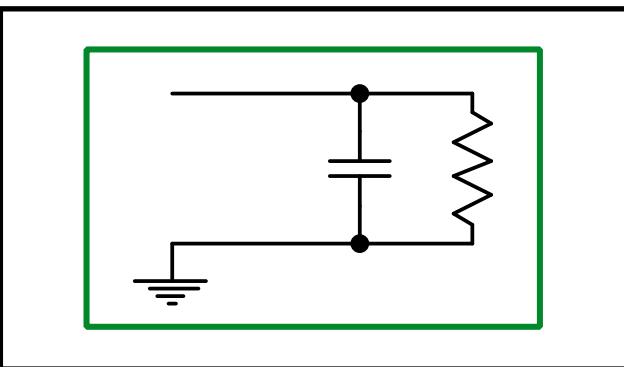
Output values
systolic BP,
diastolic BP



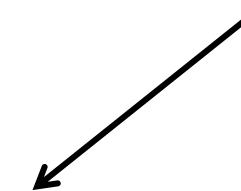
Virtual population

Parameters

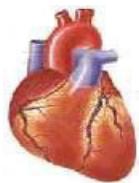
$$P_{out}, C, \tau$$



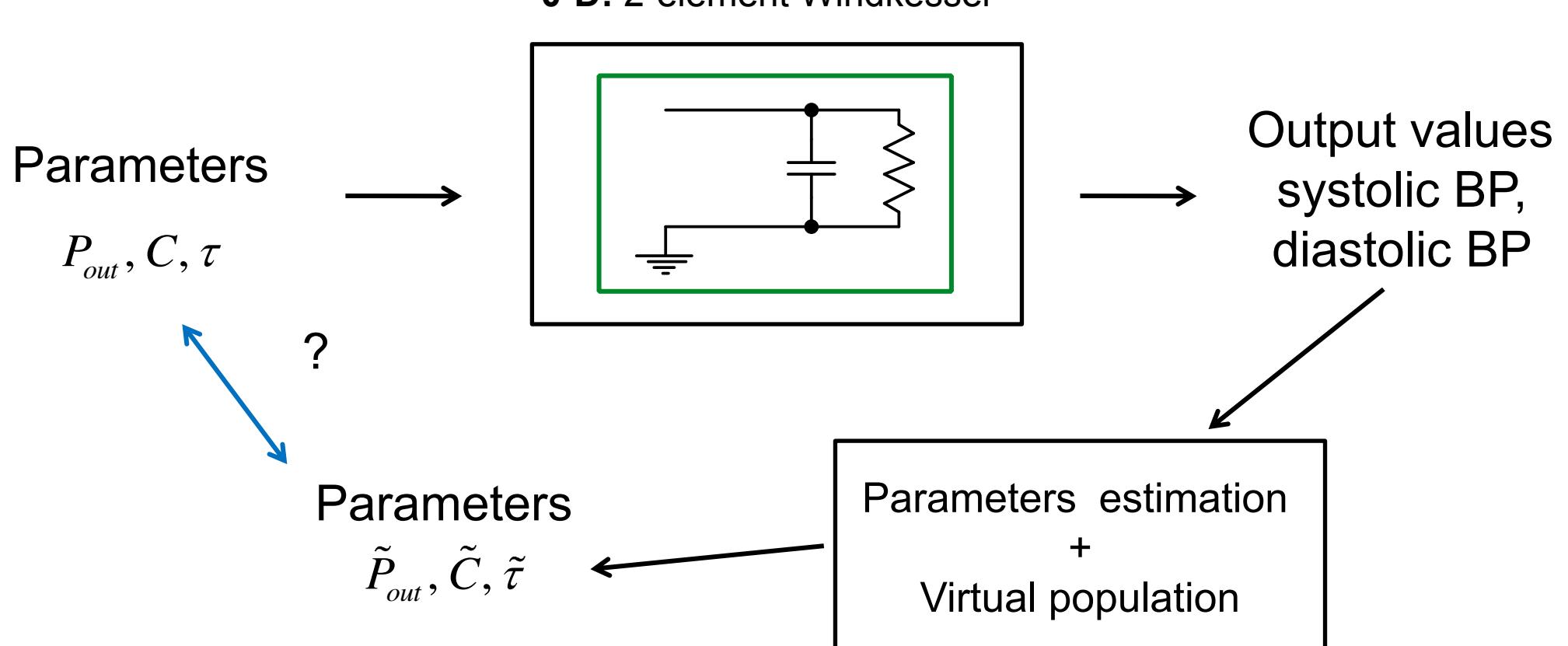
Output values
systolic BP,
diastolic BP



Parameters estimation
+
Virtual population

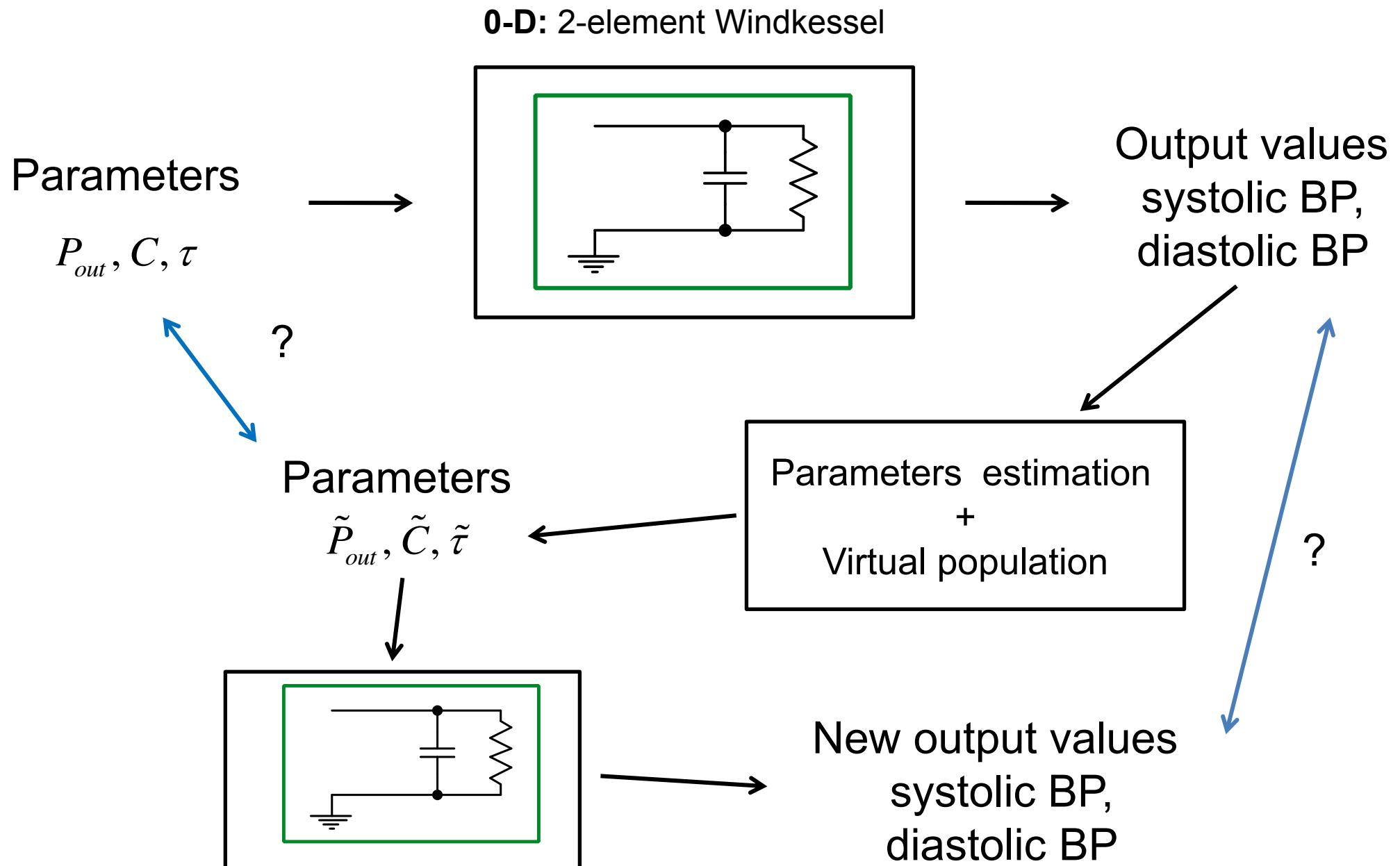


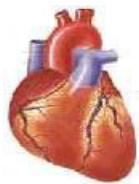
Virtual population



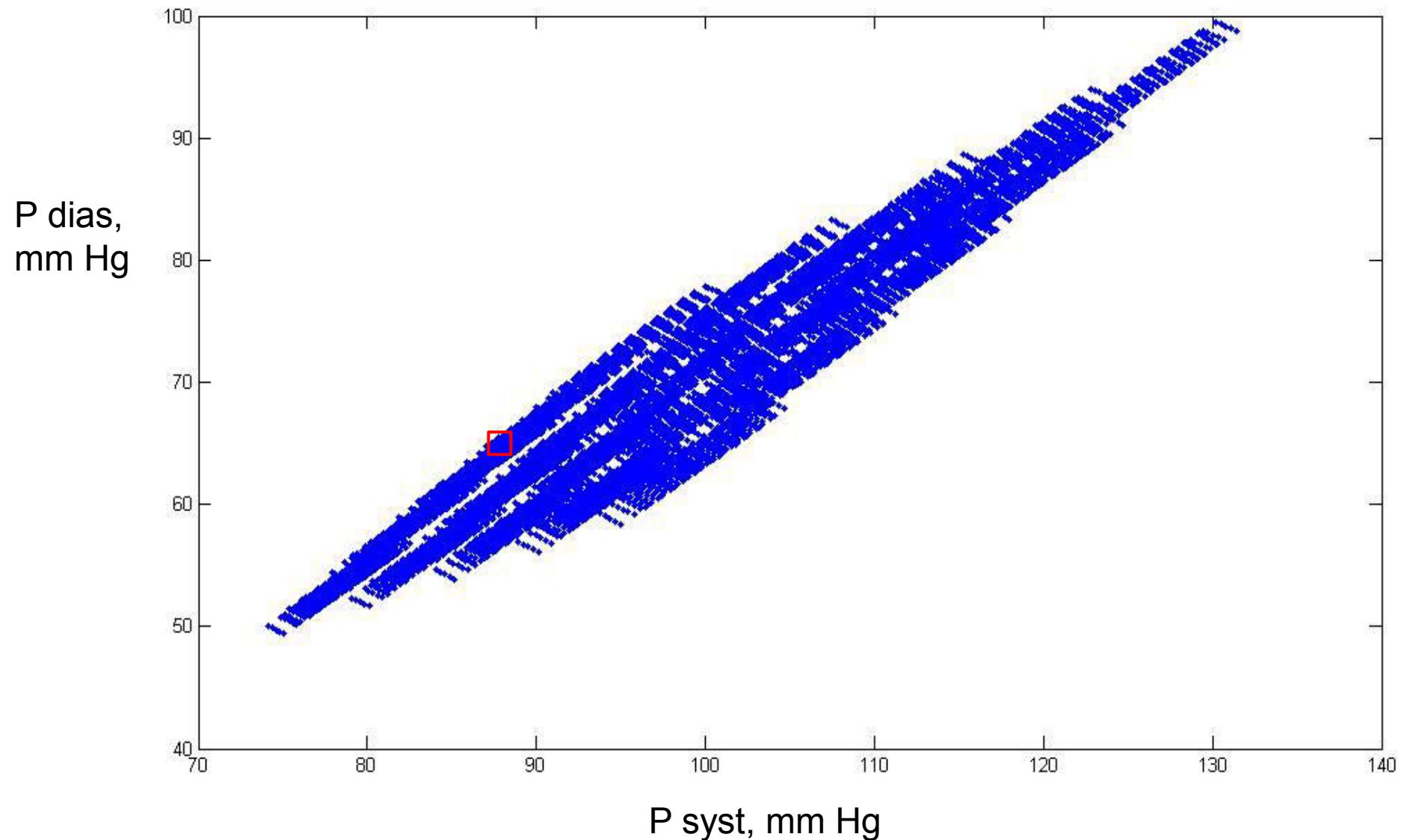


Virtual population



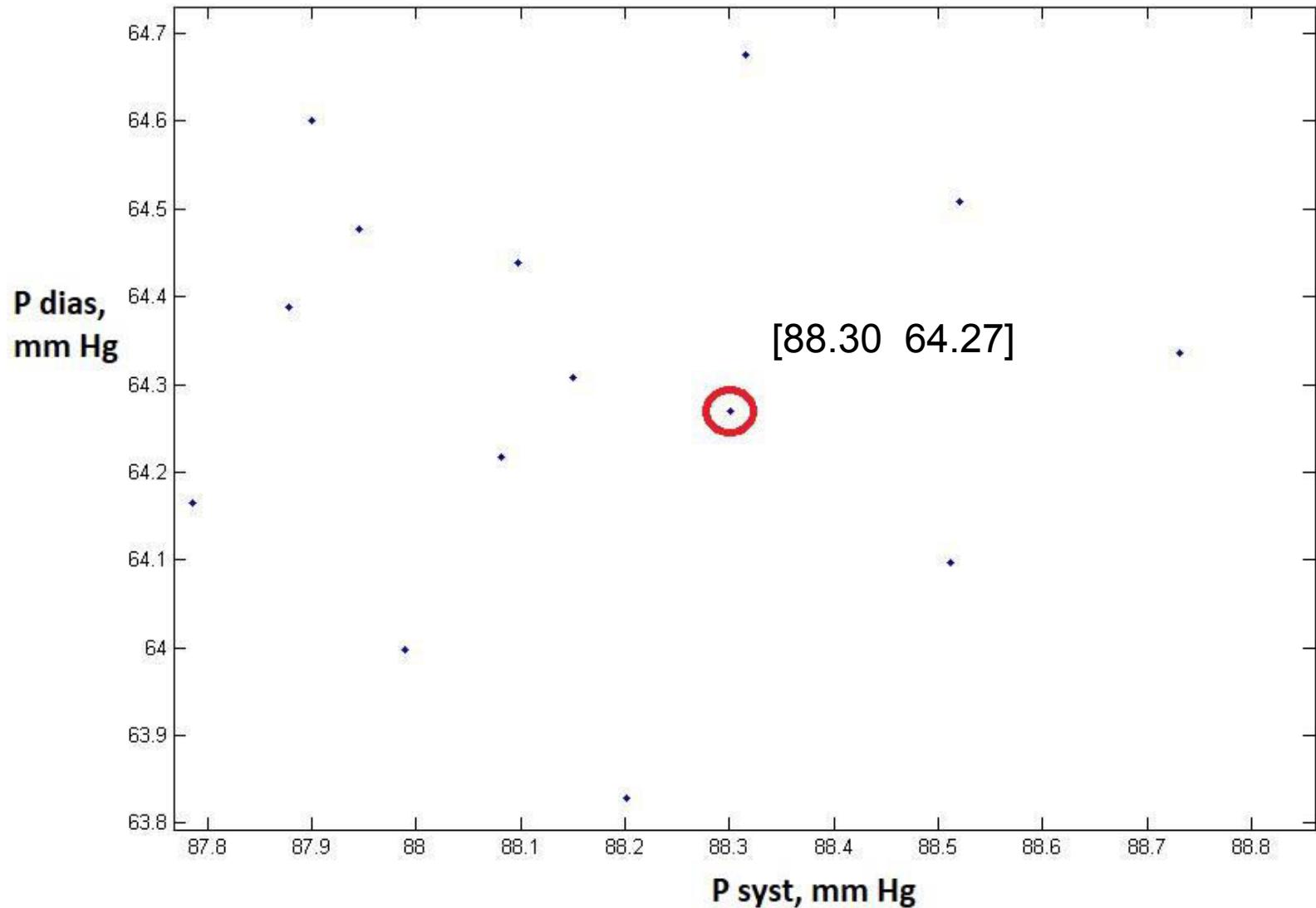


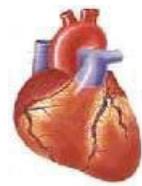
Virtual population pressures distribution



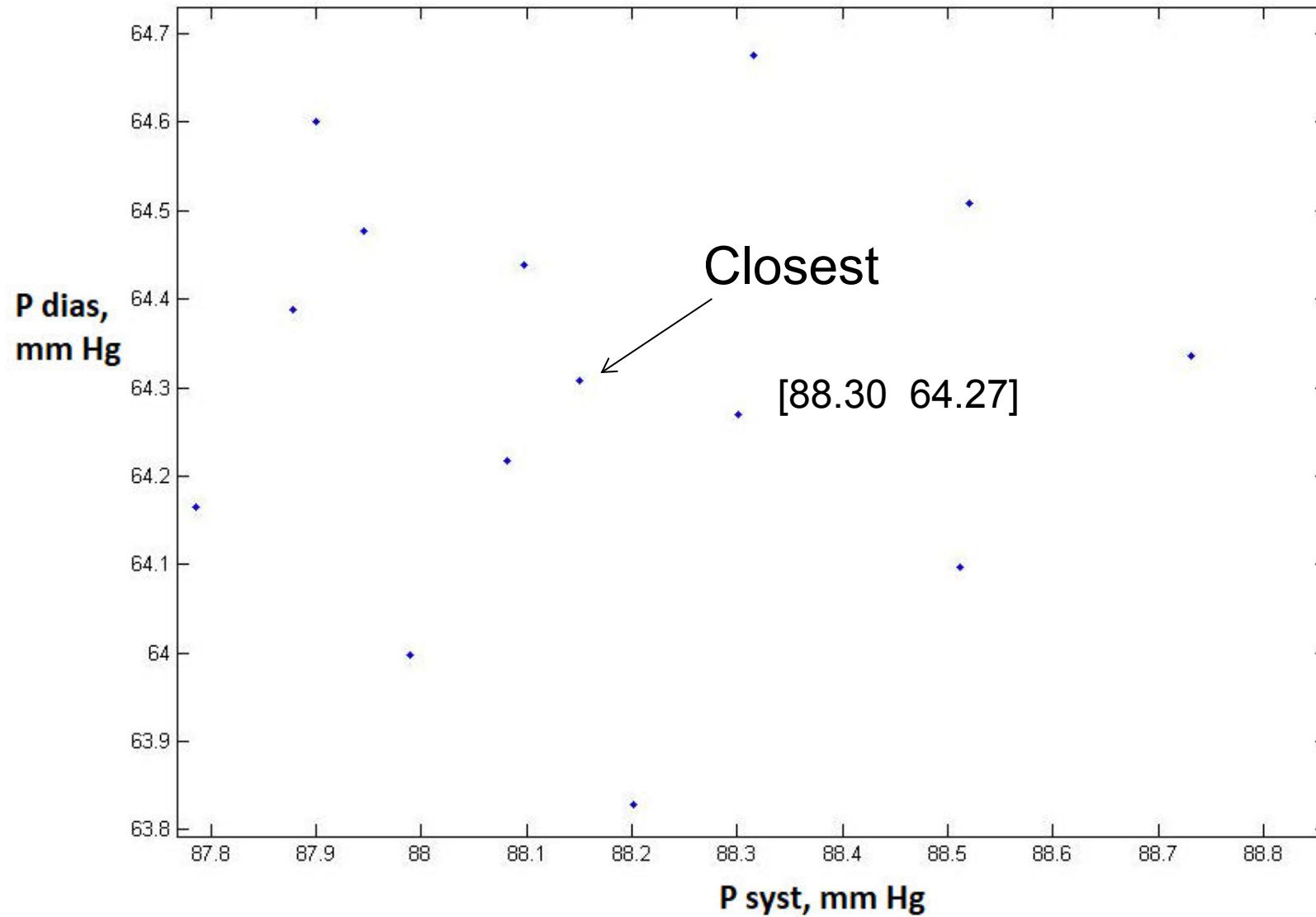


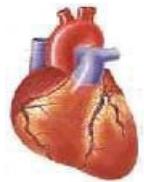
Virtual population pressures distribution



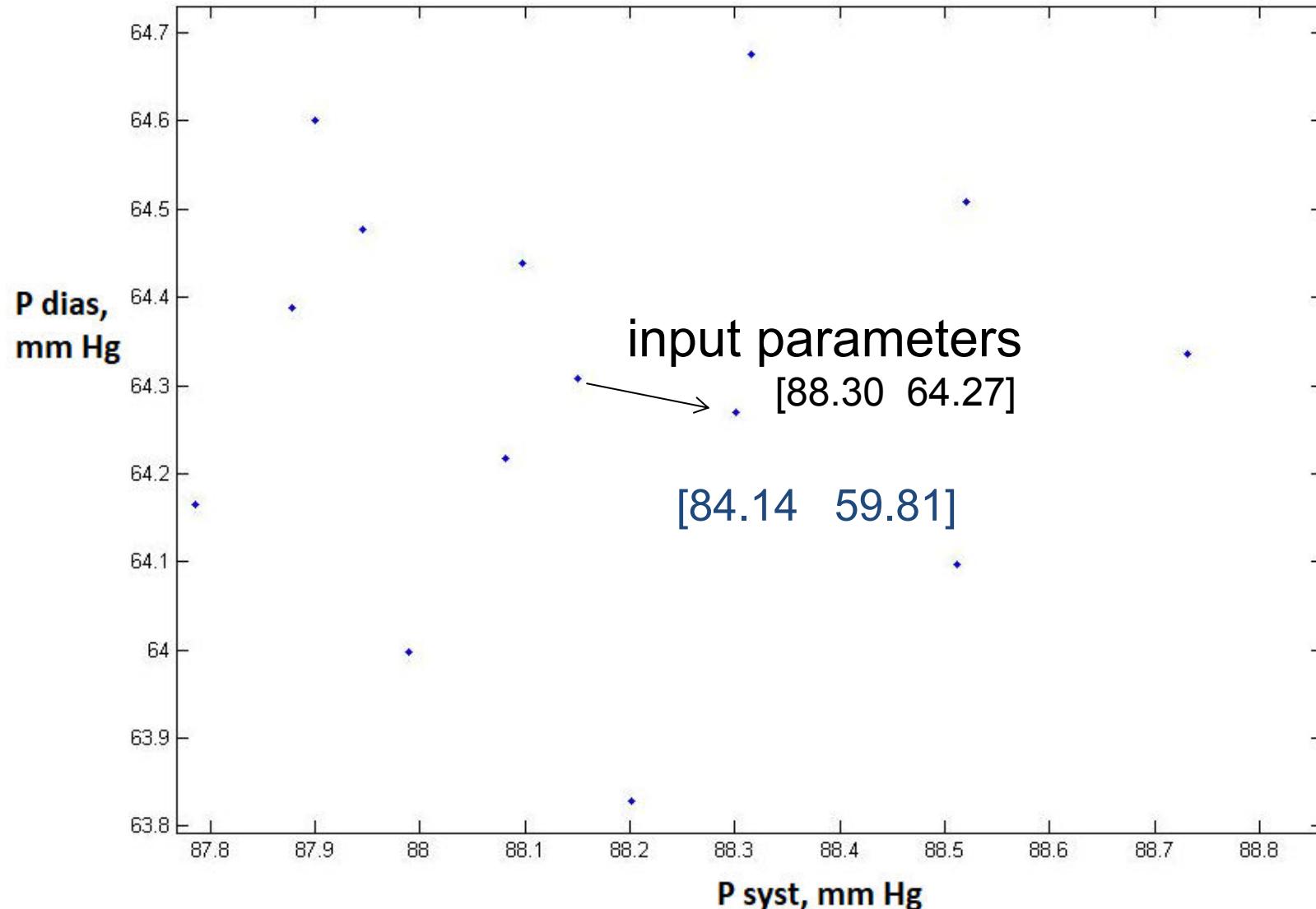


Virtual population pressures distribution



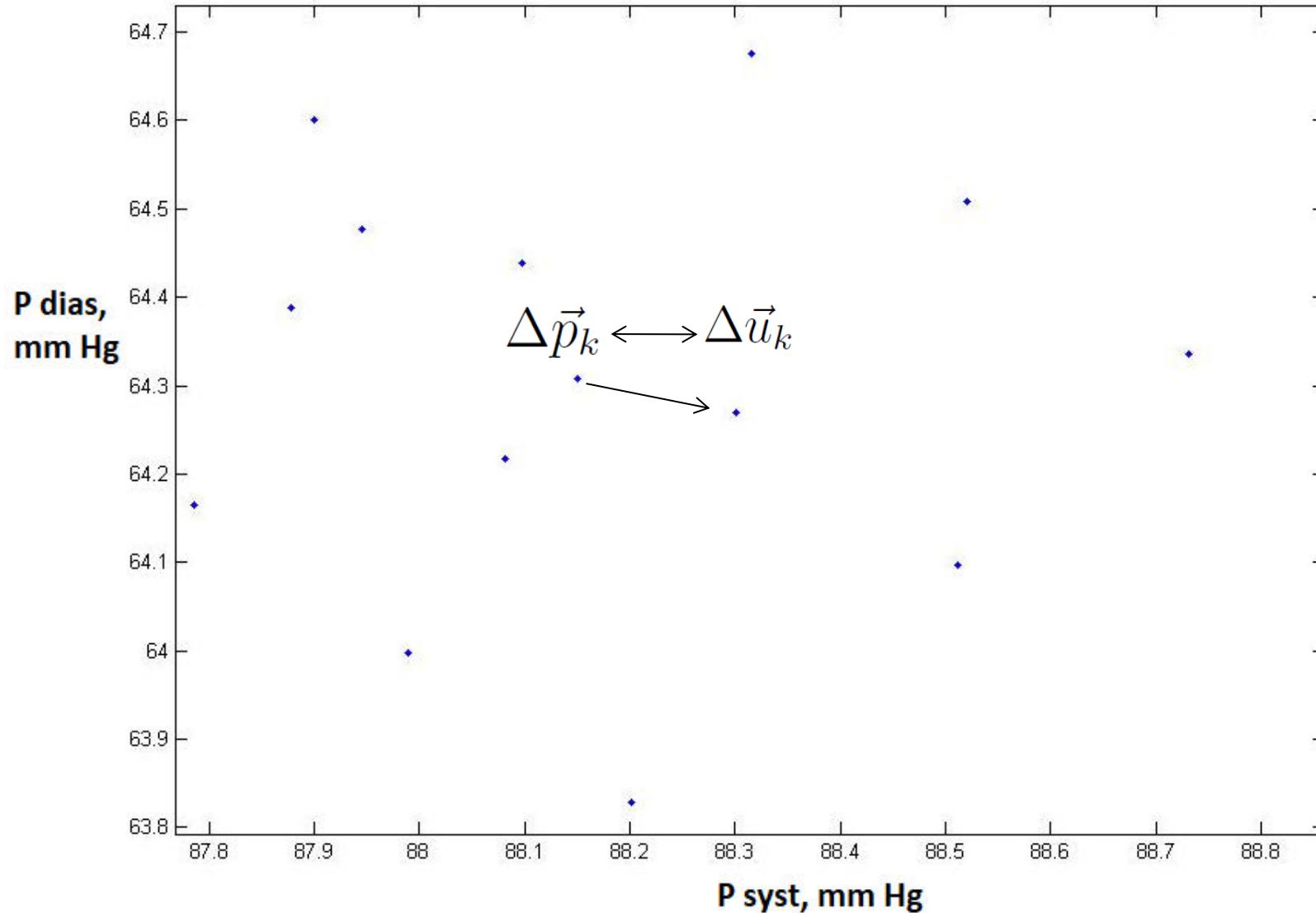


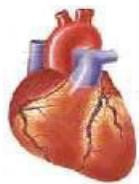
Take parameters from the closest point



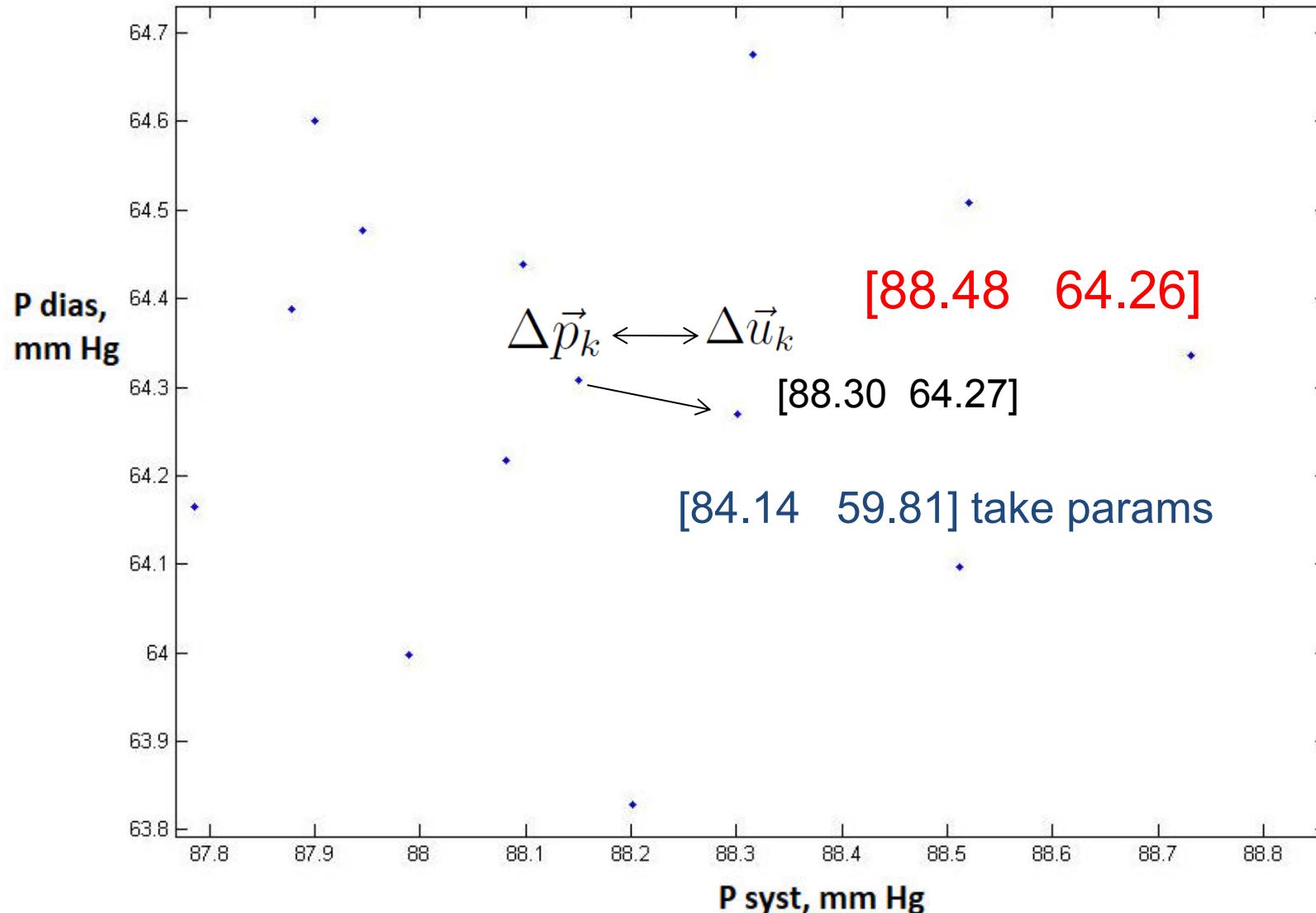


Use parameters estimation algorithm



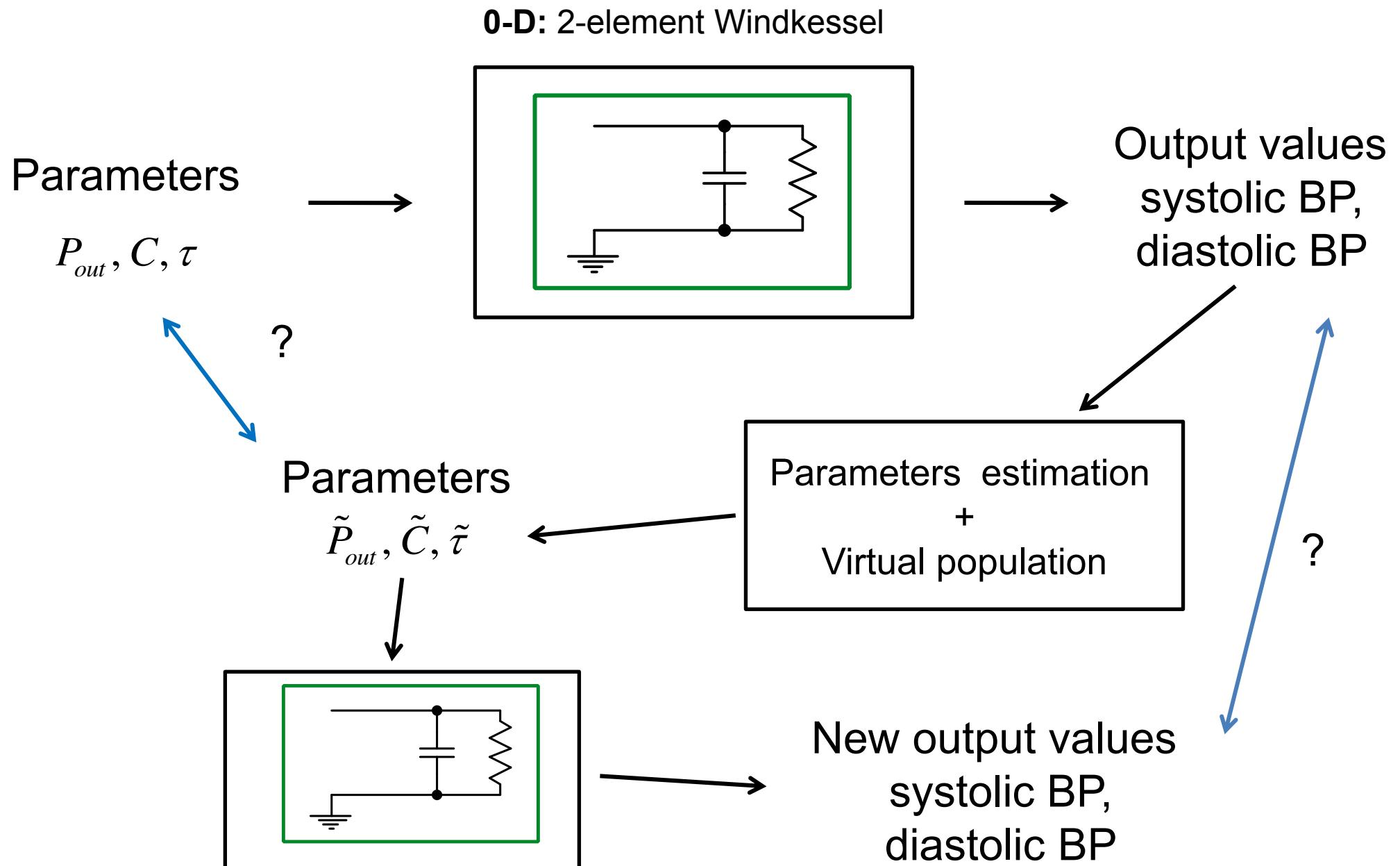


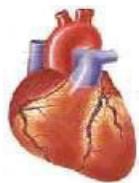
Use parameters estimation algorithm





Virtual population





All virtual population

	Relative deviation	
	max	average
<i>Output values (P syst, P diast)</i>		
Transfer parameters	10 %	2 %
Parameters estimation	0.8 %	0.2 %
<i>Input parameters</i>		
P_{out}, C, τ		
Transfer parameters	17 %	7 %
Parameters estimation	16 %	5 %



Conclusion



Pros

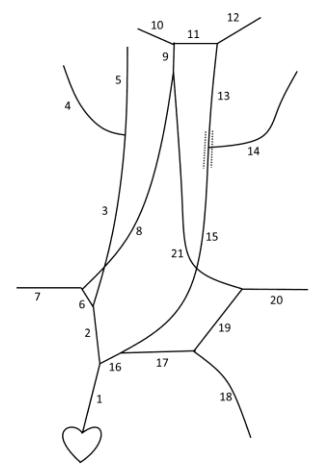
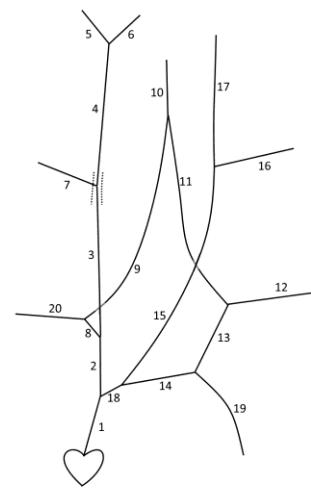
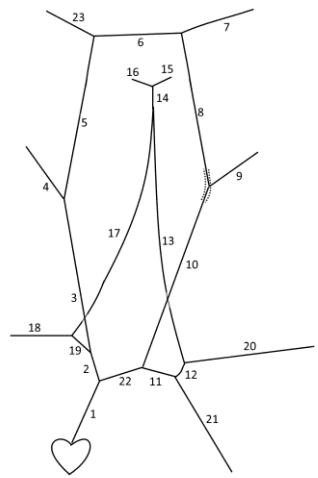
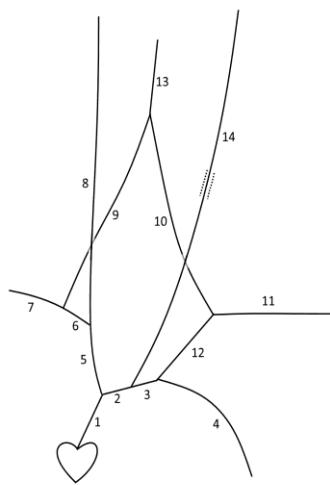
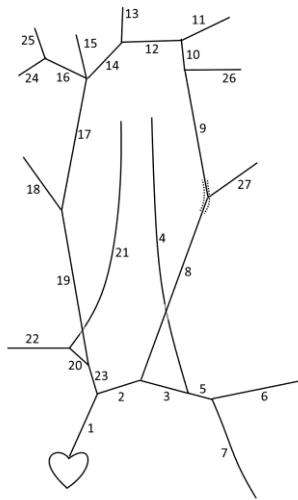
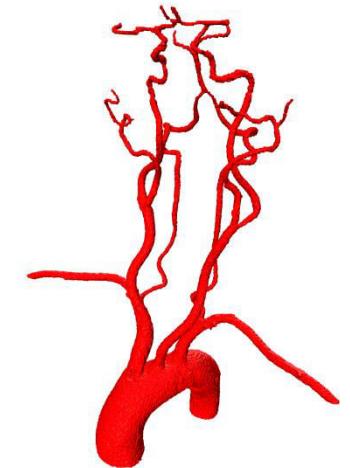
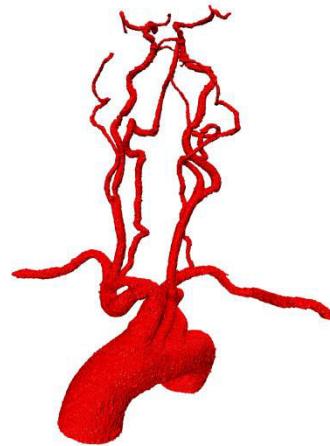
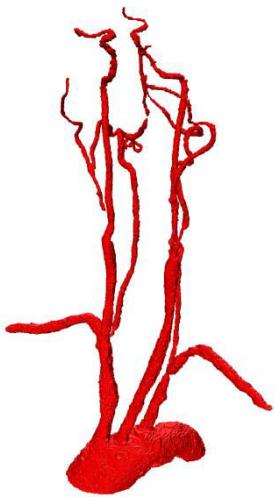
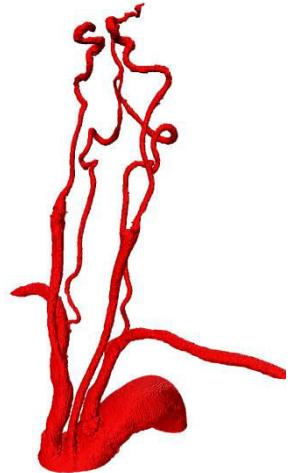
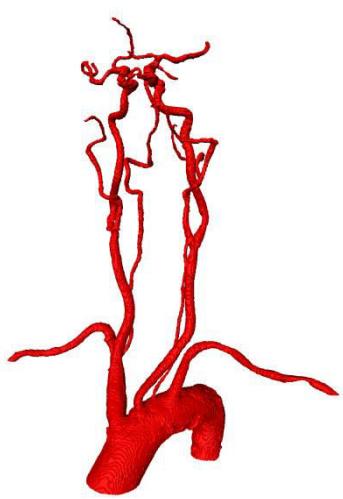
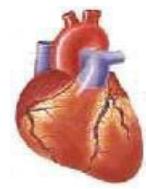
- fast
- can handle problems with a lot of parameters
- good for similar problems

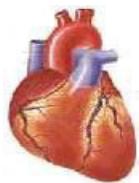
Cons

- nonlinearity
- low accuracy



Thank You!





Blood flow circulation model

1) Mass balance

$$\frac{\partial A}{\partial t} + \frac{\partial(uA)}{\partial x} = 0$$

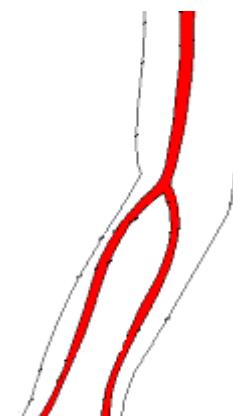
2) Momentum balance

$$\frac{\partial u}{\partial t} + \frac{\partial}{\partial x} \left(\frac{u^2}{2} + \frac{P}{\rho} \right) = -16\mu u \frac{\eta(A)}{Ad^2} + \psi(\dots), \quad \eta(A) = \begin{cases} 2, & A > A_0 \\ \frac{A}{A_0} + \frac{A_0}{A}, & A \leq A_0 \end{cases}$$

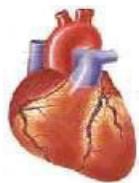
3) Bifurcations

$$3.1 \quad \sum_{k=k_1, \dots, k_M} \varepsilon_k^m Q_k = 0, \quad \varepsilon_k^m = \pm 1, \quad Q_k = u_k A_k$$

$$3.2 \quad p_k + \frac{\rho u_k^2}{2} = p_j + \frac{\rho u_j^2}{2}, \quad \forall j, k$$



3.3 Compatibility conditions



Wall state equation

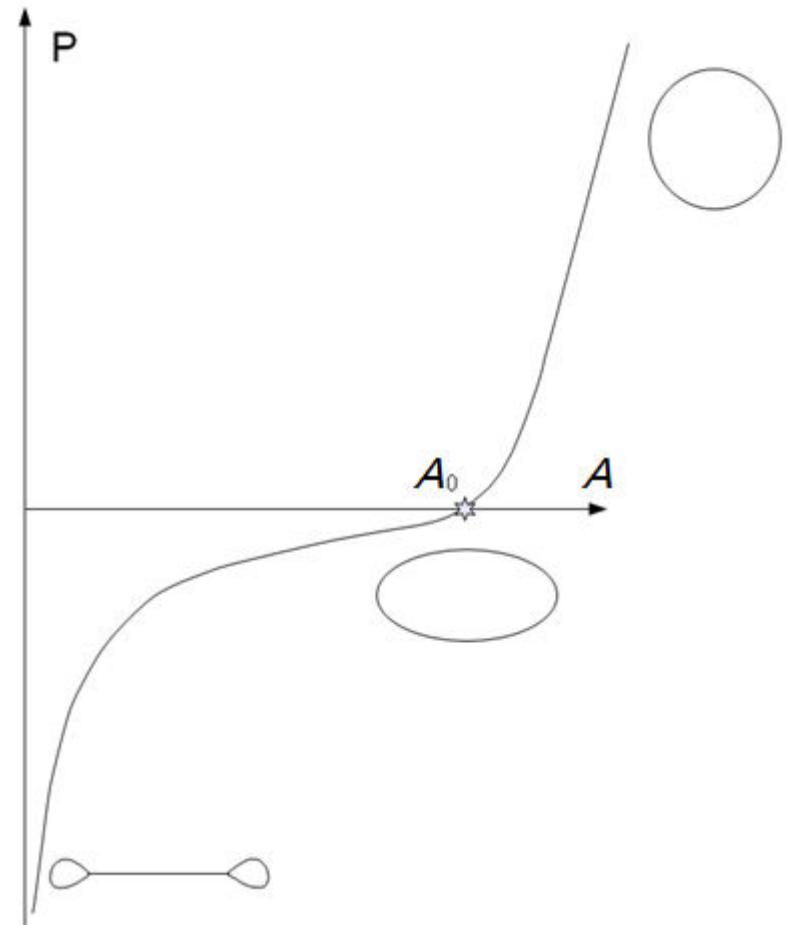
4) Vessel wall elasticity

Analytic approximation

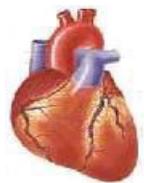
$$P(A) = P^{ext}(t, x) + \rho c^2 f(A)$$

$$f(A) = \begin{cases} \exp(A/A_0 - 1) - 1, & A > A_0 \\ \ln(A/A_0), & A \leq A_0 \end{cases}$$

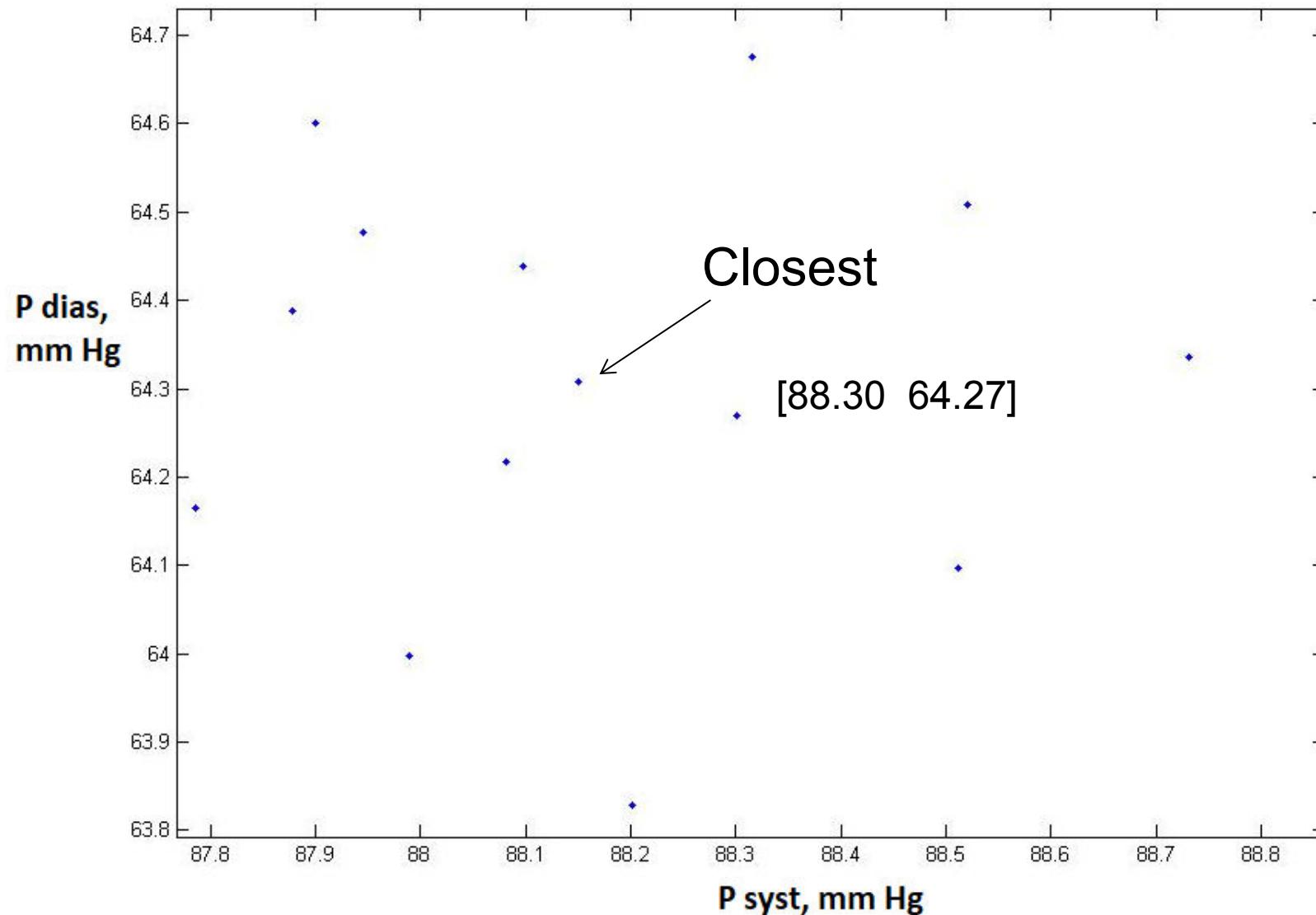
$P^{ext}(t, x)$ – external pressure



Pedley, Luo, 1998



Virtual population pressures distribution

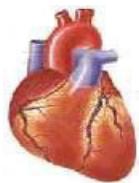




Closest:

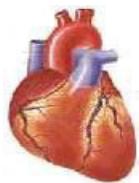
{P syst, P diast, CA}





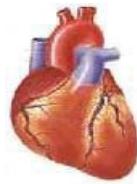
All virtual population

	Relative deviation	
	max	average
<i>Output values (P syst, P diast)</i>		
Transfer parameters	10 %	2 %
Parameters estimation	0.8 %	0.2 %
<i>Input parameters</i>		
P_{out}, C, τ		
Transfer parameters	17 %	7 %
Parameters estimation	16 %	5 %



All virtual population 3Wk

	Relative deviation	
	max	average
<i>Output values</i> <i>(P syst, P diast)</i>		
Transfer parameters	5 %	0.4 %
Parameters estimation	5 %	0.4 %
<i>Input parameters</i> <i>P_{out}, C, τ, Z₀</i>		
Transfer parameters	15 %	6 %
Parameters estimation	15 %	6 %



All virtual population 3Wk ($R > 10R_{min}$)



Relative deviation

<i>Output values (P_{syst}, P_{diast})</i>	max	average
Transfer parameters	16 %	3 %
Parameters estimation	7 %	2 %
<i>Input parameters</i>		
P_{out}, C, τ, Z_0		
Transfer parameters	40 %	9 %
Parameters estimation	50 %	6 %



- CA from pressure wave (paper)
- Response surface model